- 1.1 Characterize and correct for B1 field inhomogeneity
- 1.2 Reduce distortion due to B0 field inhomogeneity
- 1.3 Real-time correction of head motion during scanning
- 1.4 Characterize and correct for gradient distortions
- 1.5 Continue with the calibration of T1 acquisitions

- 1.1 Characterize and correct for B1 field inhomogeneity
- 1.2 Reduce distortion due to B0 field inhomogeneity
- 1.3 Real-time correction of head motion during scanning
- 1.4 Characterize and correct for gradient distortions
- 1.5 Continue with the calibration of T1 acquisitions

B₁ Inhomogeneity Dielectric Resonance at 3T



MP_RAGE

T₁-weighted GRE TR=20ms, FA=30deg PD-weighted GRE TR=20ms, FA=5deg

B₁ Inhomogeneity Dielectric Resonance Effects at 3T



Estimated B₁ Transmit Map at 3T

B₁ Inhomogeneity Correction for Dielectric Resonance Effects at 3T





MP-RAGE

B₁ corrected Synthetic T1-weighted

B₁ Inhomogeneity Correction for Dielectric Resonance Effects at 3T





 B_1 corrected Synthetic T_1 -weighted B₁ corrected Synthetic "PD-weighted"

- 1.1 Characterize and correct for B1 field inhomogeneity
- 1.2 Reduce distortion due to B0 field inhomogeneity
- 1.3 Real-time correction of head motion during scanning
- 1.4 Characterize and correct for gradient distortions
- 1.5 Continue with the calibration of T1 acquisitions

Spatial Distortion due to Magnetic Susceptibility (B₀) Pulse-Sequence Dependence (S/I readout direction)



Spatial Distortion due to Magnetic Susceptibility (B₀) Pulse-Sequence Dependence (I/S readout direction)



Multi-Echo 3-D FLASH/SPGR Sequence

5 deg Flip angle

30 deg Flip angle







Reduction of Scan-Rescan Variance



Overlay threshold: 8%

- 1.1 Characterize and correct for B1 field inhomogeneity
- 1.2 Reduce distortion due to B0 field inhomogeneity
- 1.3 Real-time correction of head motion during scanning
- 1.4 Characterize and correct for gradient distortions
- 1.5 Continue with the calibration of T1 acquisitions

Rigid body motion is calculated every TR by comparing the new clover-leaf navigator with a pre-measured map of k-space in the vicinity of the target navigator









K-space values in vicinity of octant navigator

Andre van der Kouwe, MGH

Real-Time Motion Tracking using Cloverleaf Navigators



Without motion correction

With real-time motion correction

Andre van der Kouwe, MGH

With navigator motion correction it was possible to collect high resolution structural scans of the amnesic patient H.M.





3D FLASH (TR=20 ms, TE=10 ms, 1.3 x 1 x 1.3 mm, Tacq=7:45, BW=160 Hz/pixel, 6 averages)

- 1.1 Characterize and correct for B1 field inhomogeneity
- 1.2 Reduce distortion due to B0 field inhomogeneity
- 1.3 Real-time correction of head motion during scanning
- 1.4 Characterize and correct for gradient distortions
- 1.5 Continue with the calibration of T1 acquisitions

Gradient Nonlinearity Distortion Uncorrected Phantom Data

GE Whole-Body CRM NVi/CVi

Siemens Whole-Body Symphony/Sonata

Brain Morphometry BIRN: MGH, BWH, Duke, UCSD, UCI, UCLA

Gradient Nonlinearity Distortion Corrected Phantom Data

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GE Whole-Body CRM NVi/CVi

Siemens Whole-Body Symphony/Sonata

Brain Morphometry BIRN: MGH, BWH, Duke, UCSD, UCI, UCLA

Gradient Nonlinearity Distortion Uncorrected



ADNI Prep Phase: Mayo Clinic, UCSD, MGH P41

Gradient Nonlinearity Correction Corrected



ADNI Prep Phase: Mayo Clinic, UCSD, MGH P41