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# Geometric correspondence

Guido Gerig, Utah II

Polina Golland, MIT

Martin Styner, UNC

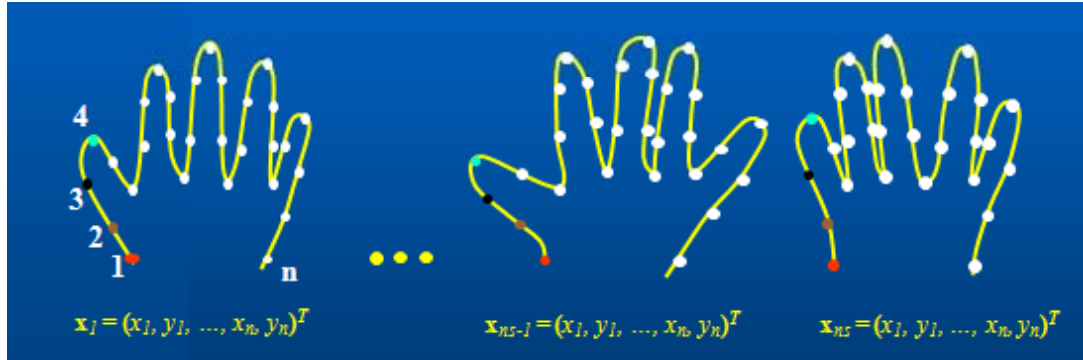
Allen Tannenbaum, GT

Ross Whitaker, Utah I

Engineering Core



# Geometric Correspondence: Shapes



Finding point to point correspondence for shape modeling and analysis

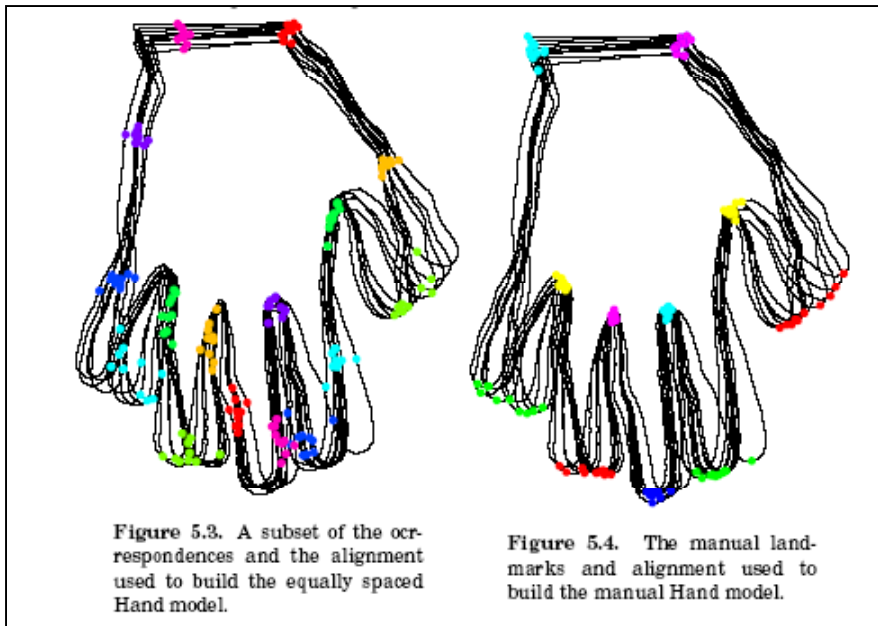
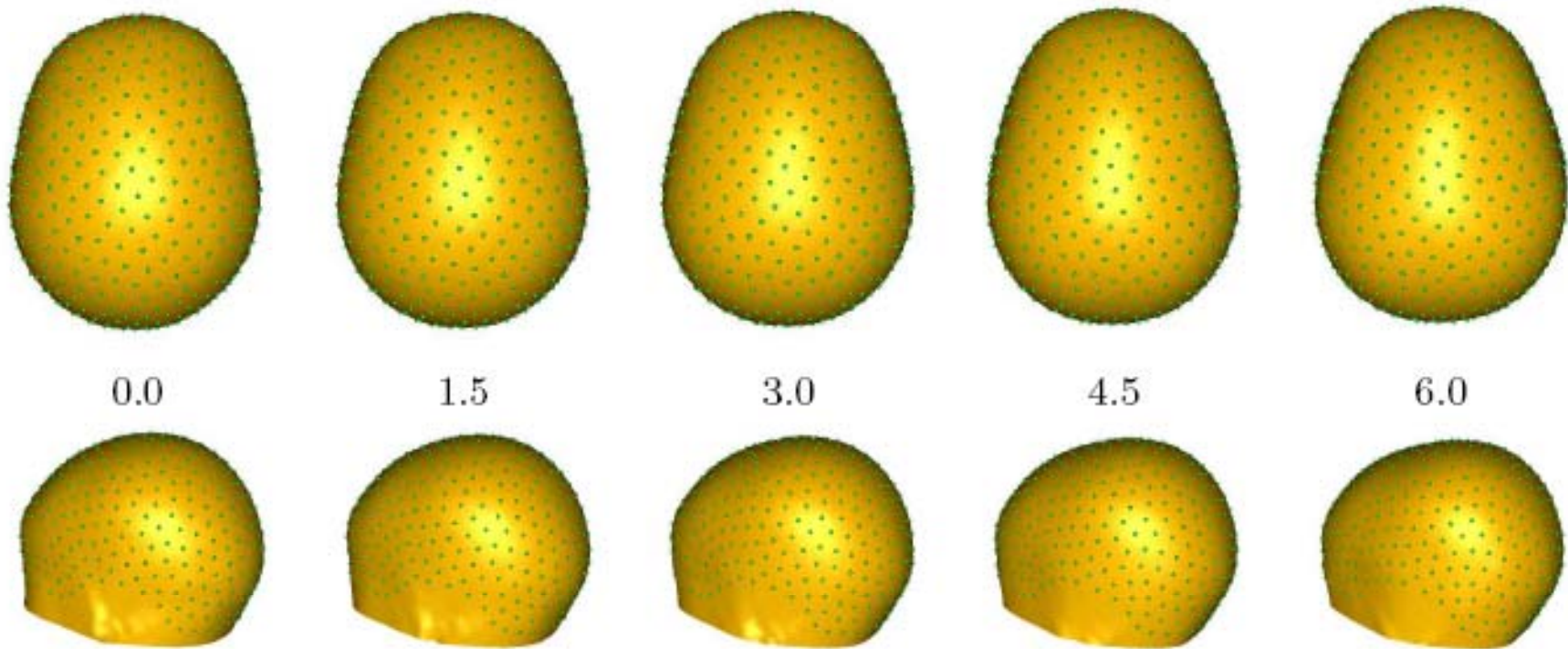


Figure 5.4. The manual landmarks and alignment used to build the manual Hand model.

<http://na-mic.org>



# Geometric Correspondence: Shapes

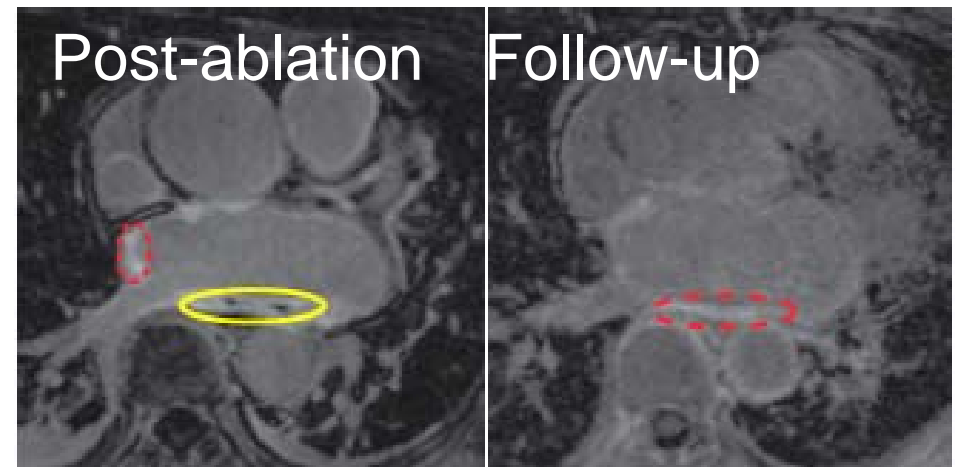
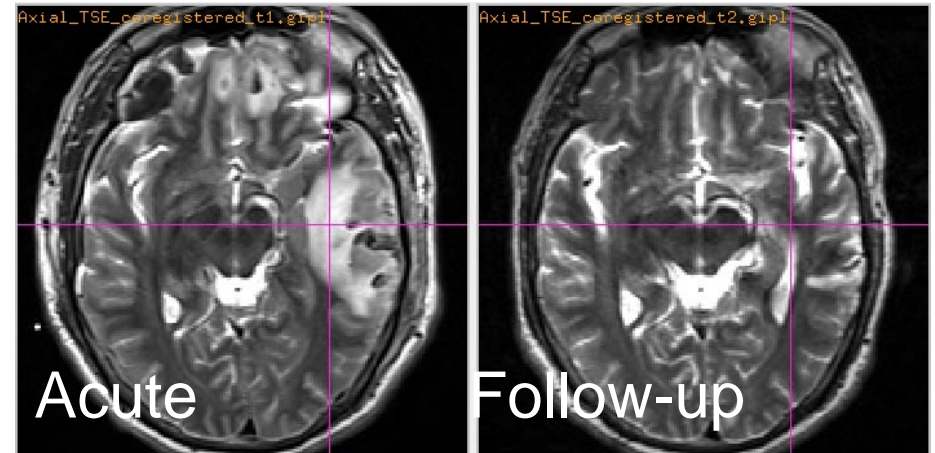


**Fig. 3.** Overview of head shape regression: Changes in head shape with age



# Dense Geometric Correspondence: Images

- Multi-modal registration
- Pre-post imaging & serial staging of individuals
- Mapping of atlas to subject: Use as prior
- Mapping image population into common coordinates: atlas
- Registration for correction of artifacts (distortion, etc.)





# Co-Registration of structural MRI: Multi-contrast analysis of tissue & pathology

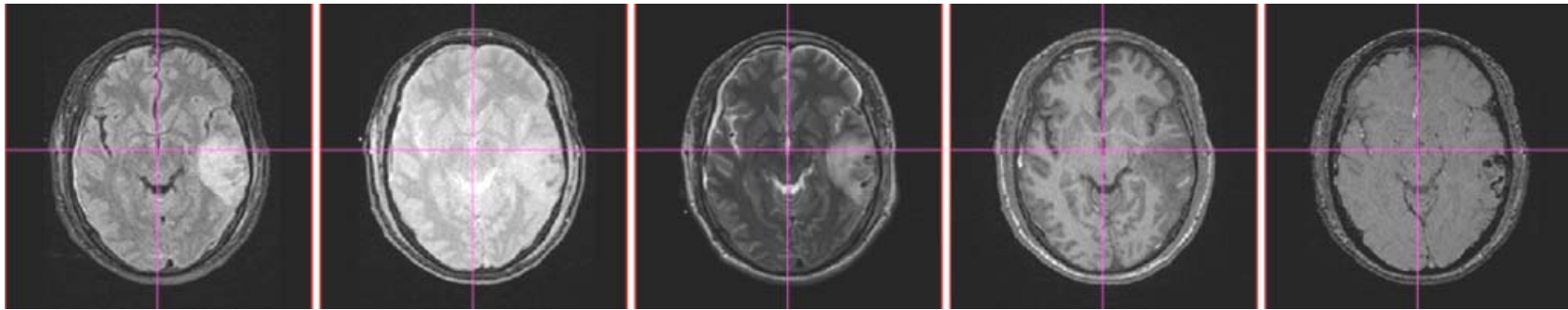
FLAIR

GRE  
-bleed

TSE

Mprage  
postcontrast

SWI



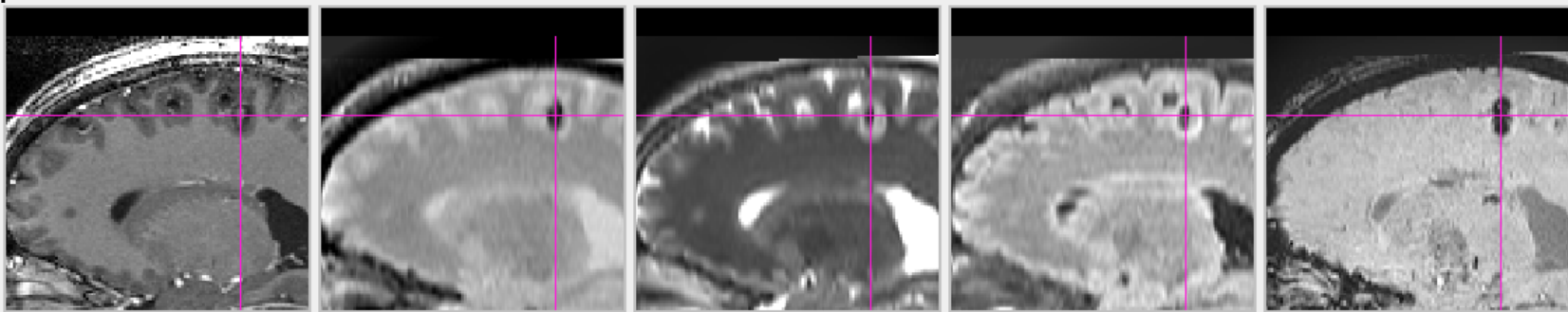
Mprage  
postcontrast

GRE-bleed

TSE

FLAIR

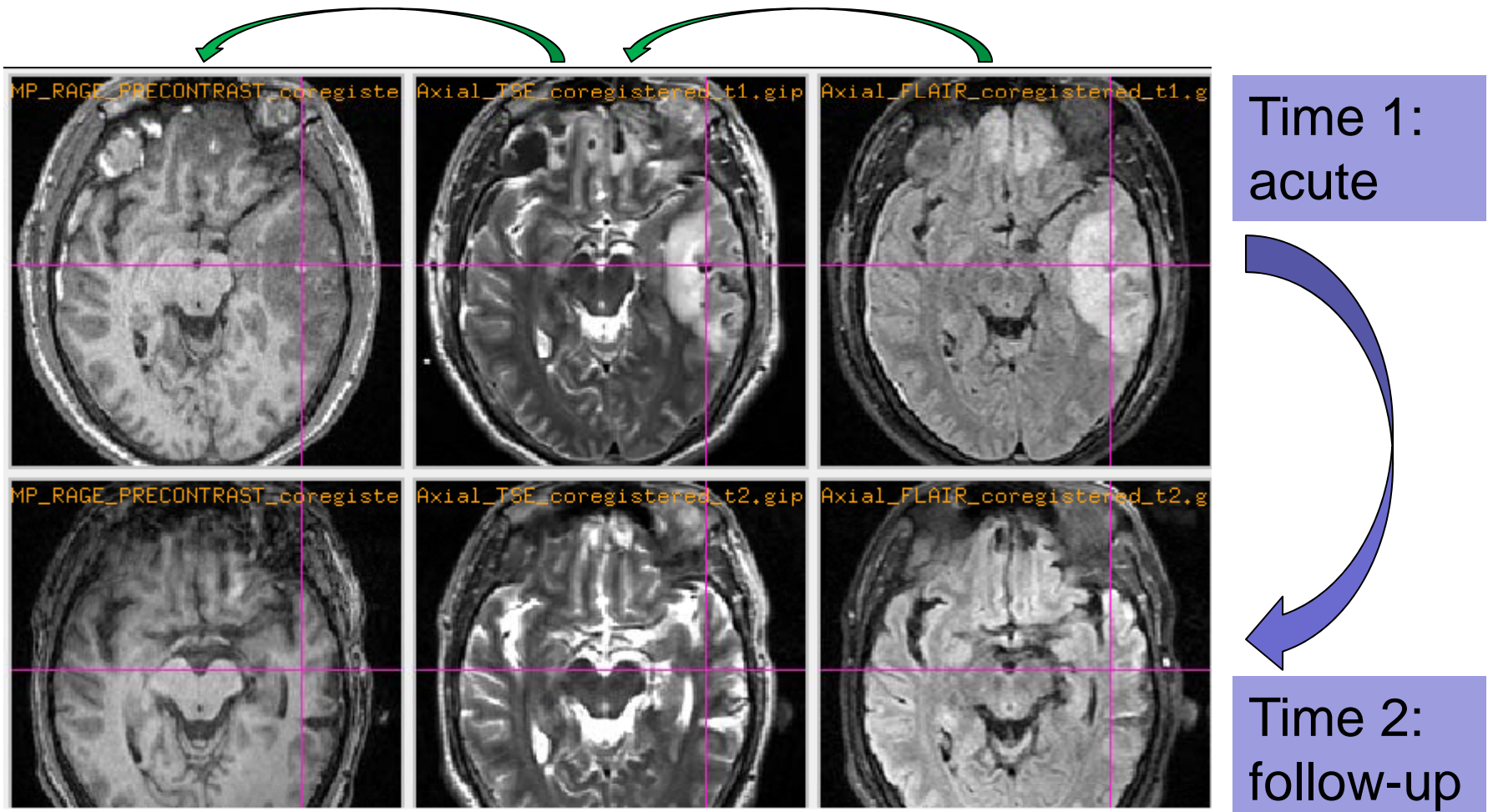
SWI



TBI case: J. Horn , Paul Vespa, D. Hovda, UCLA

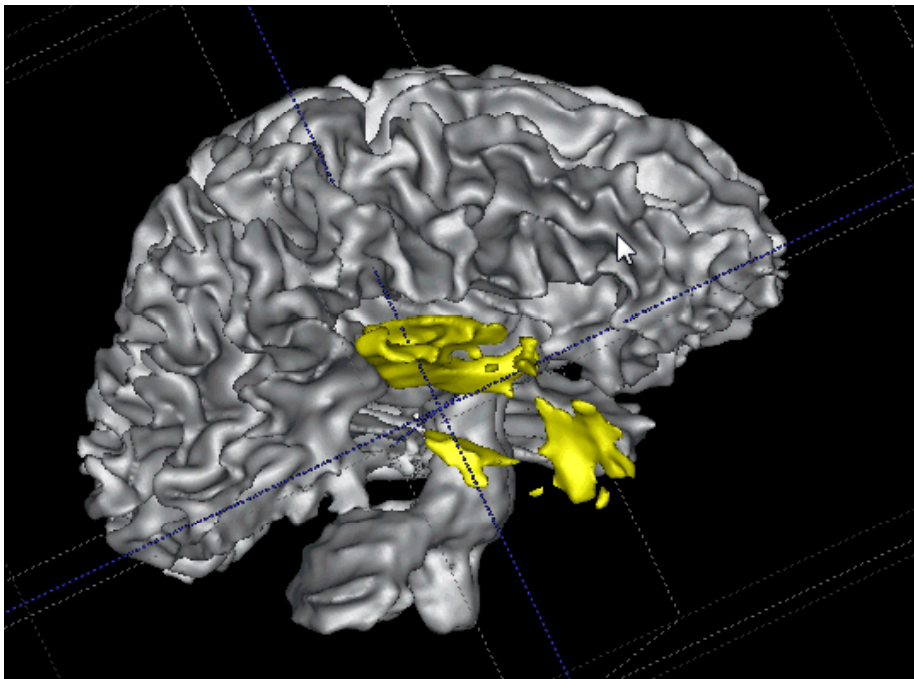


# Multi-contrast & multi-time point co-registration in presence of pathology

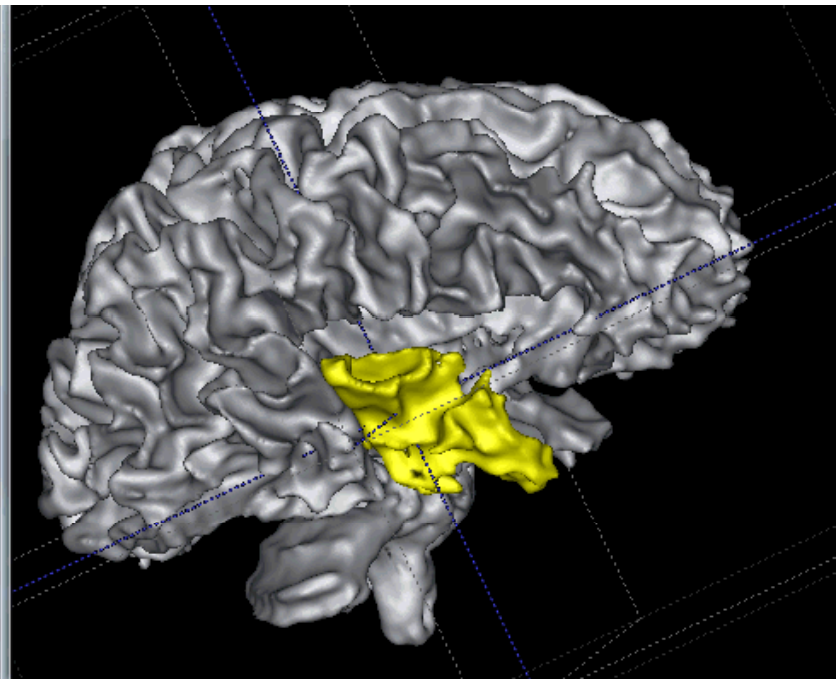




# TBI case longitudinal



acute

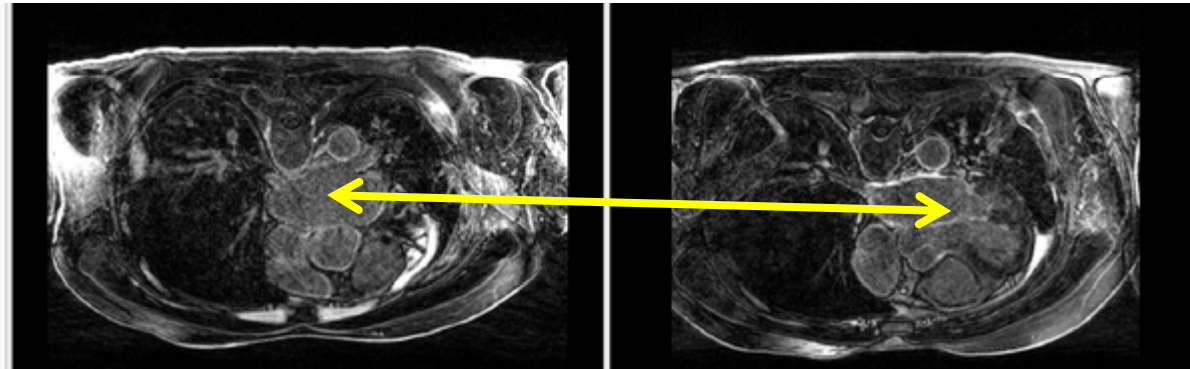


follow-up

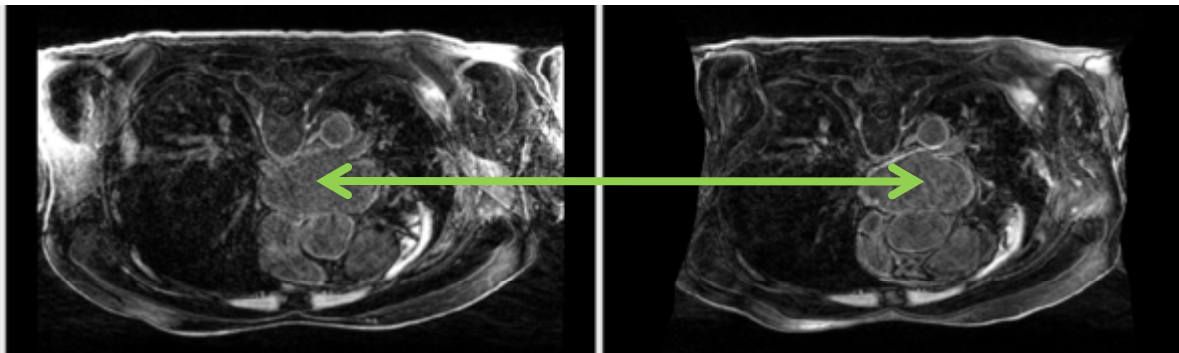
TBI case #3, multi-modal and multi-time registration,  
segmented with Slicer plug-in “ABC”



# DBP Utah: AFIB: Need for point-to-point correspondence



Before  
registration



After registration

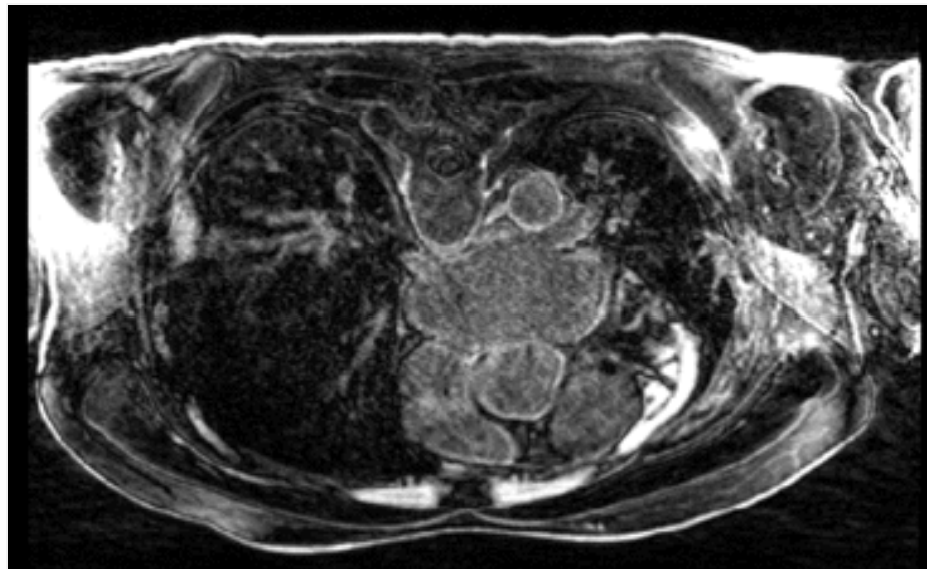
Pre-ablation

Post-ablation

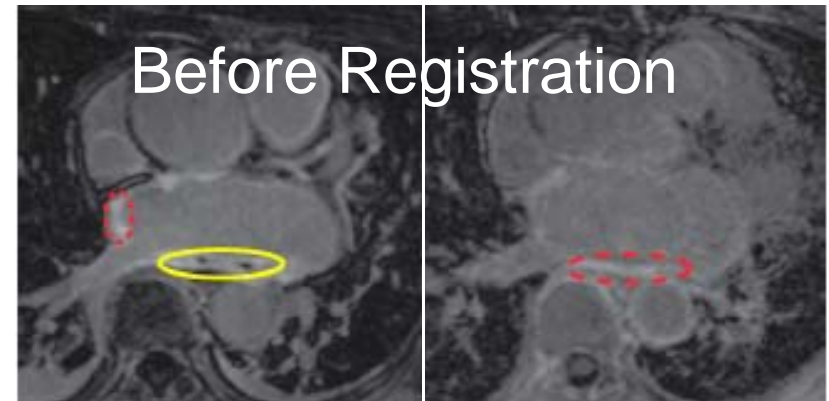




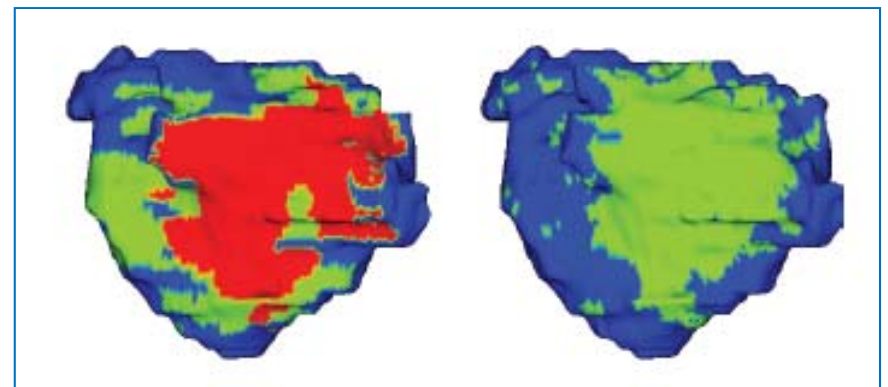
# DBP Utah: AFIB: Need for point-to-point correspondence



Pre- to Post-ablation



Post-ablation Follow-up



After registration: IPA → 3PA

JJE Blauer J Cates, CJ McGann, EG Kholmovski , A Alexander, MW Prastawa , S Joshi , NF Marrouche , RS MacLeod, [Computing in Cardiology](http://www.computingincardiology.com)

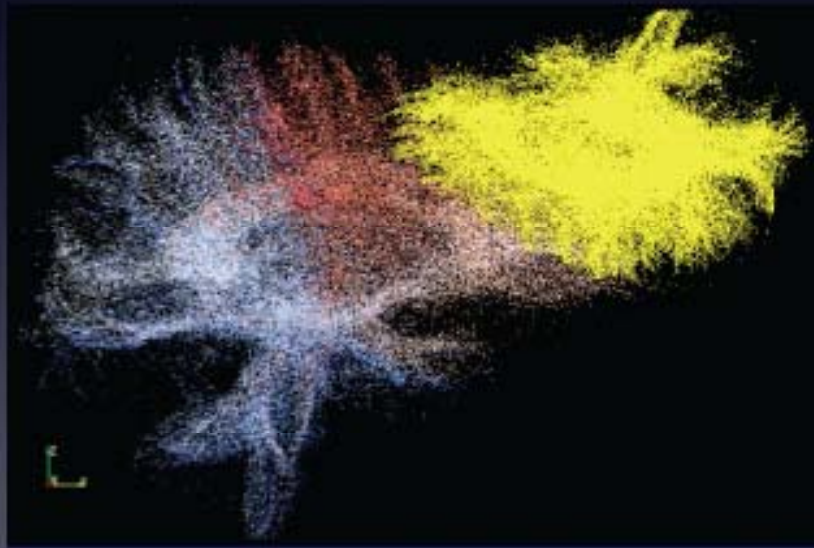
National Alliance for Medical Image Computing  
<http://na-mic.org>



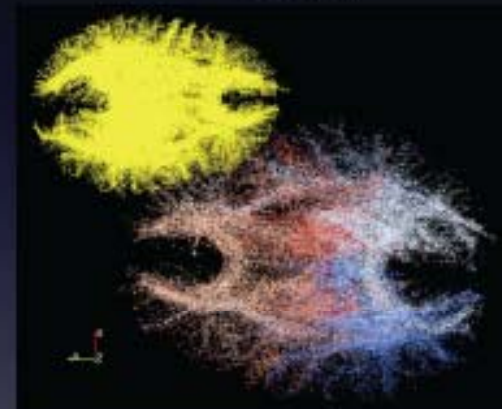
# Registration

Original Data Sets (3 Patient to Patient Sets)

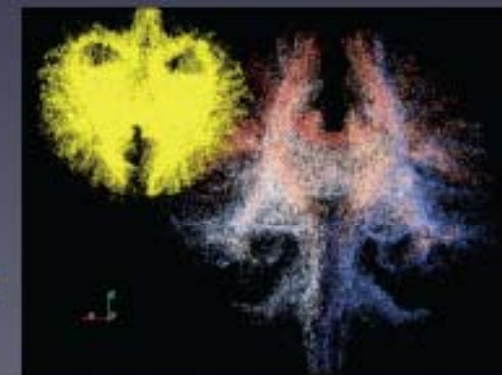
Set I



Set II



Set III

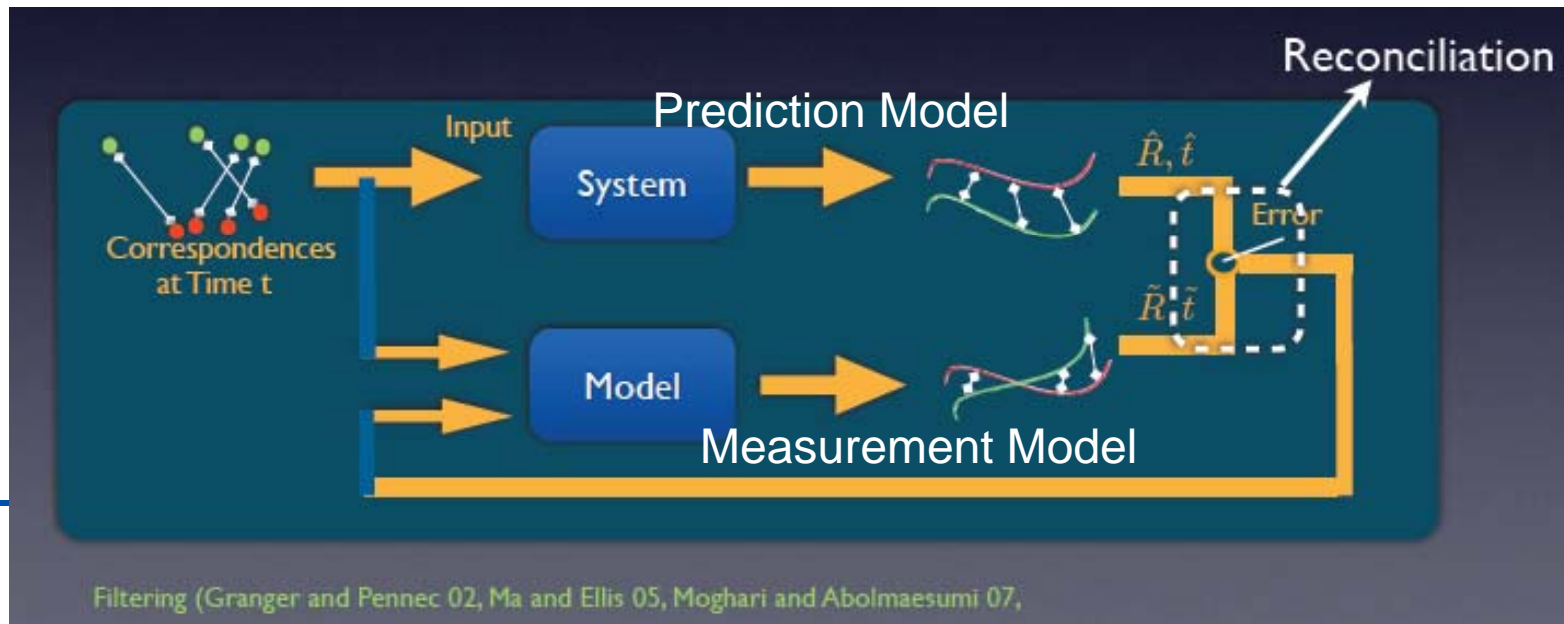


Note 1: This is on-going work done in conjunction with [Dr. Yogesh Rathl](#) at the Brigham Women's Hospital, Harvard Medical School.



# Solution via Particle Filter

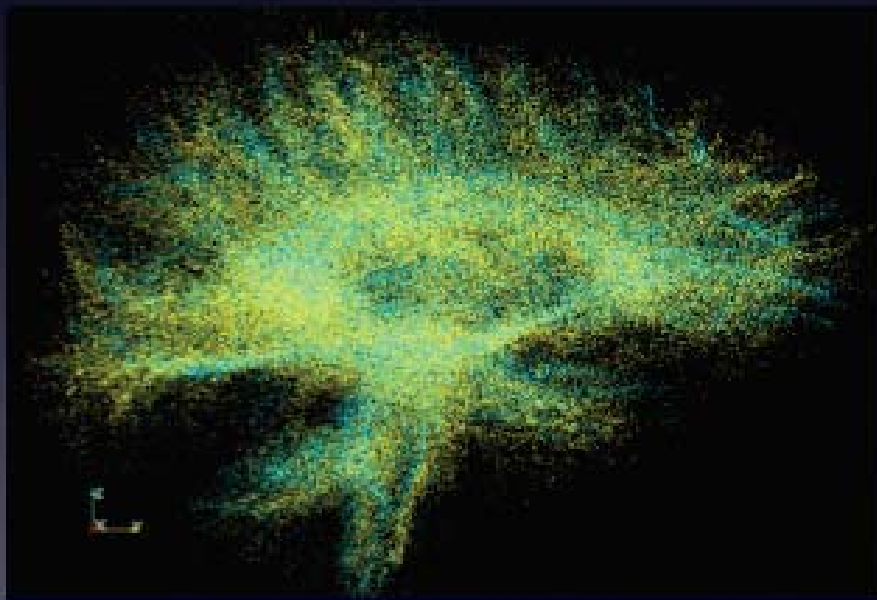
- Exists: Iterative closest points: Efficient solution?
- **New:** Consider registration as posterior estimation problem
- Hidden state variable to estimate is TRANSFORMATION
- Two part problem:
  - Establishing correspondence
  - Estimate Transformation parameters



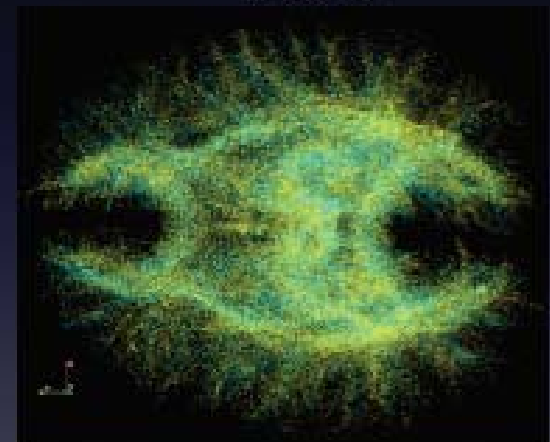
# Registration

Final Result (3 Patient to Patient Sets)

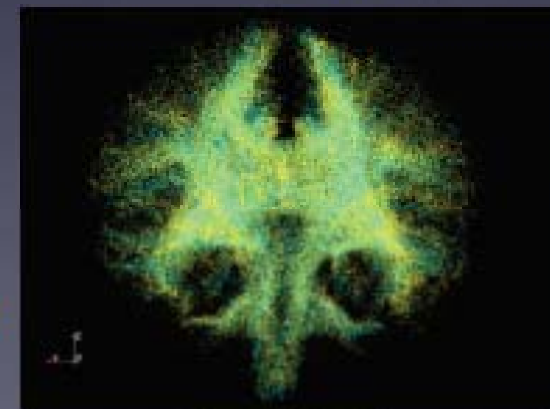
Set I



Set II



Set III

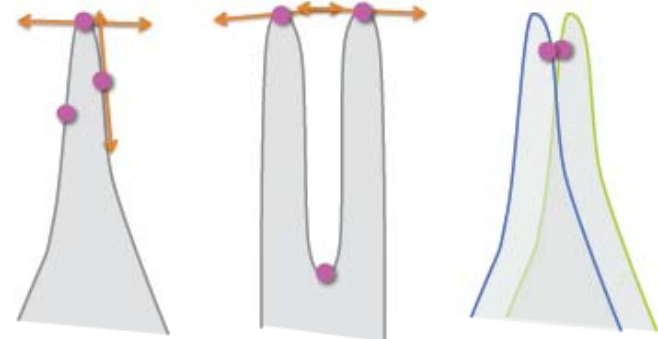
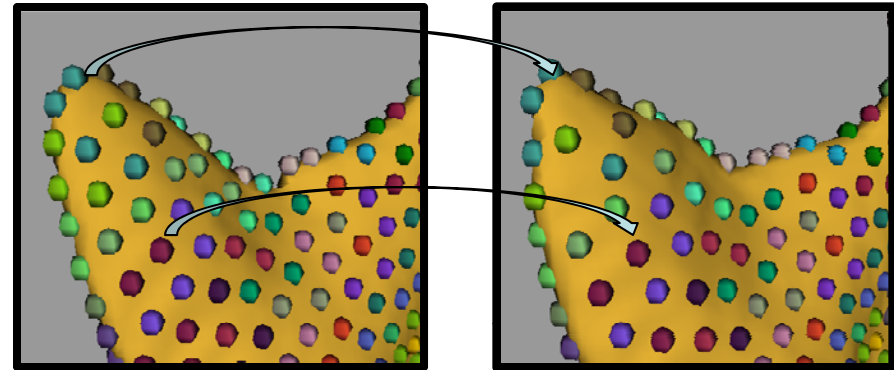


Note 1: This is on-going work done in conjunction with [Dr. Yogesh Rathl](#) at the Brigham Women's Hospital, Harvard Medical School.



# Particle Correspondence

- Particle system correspondence (Utah)
  - 2 entropy terms
    - Ensemble entropy -> how are particles similar across a set of surfaces
    - Surface entropy -> distribute the particles “evenly” across surfaces
- **Problem:** Highly convoluted surfaces (cortical surface) or very “skinny” surfaces

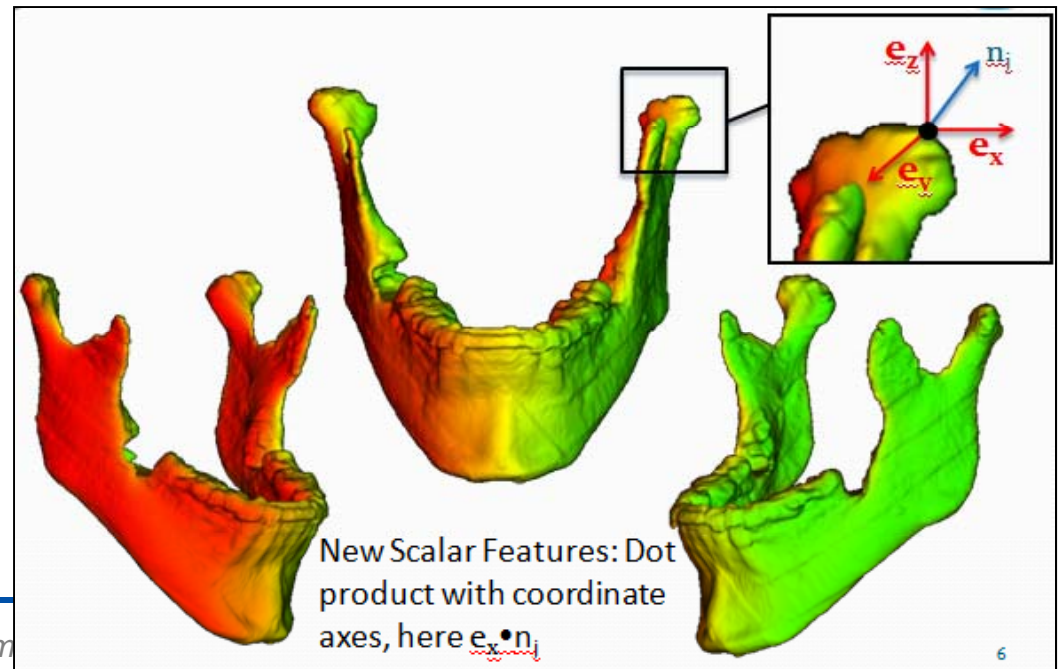
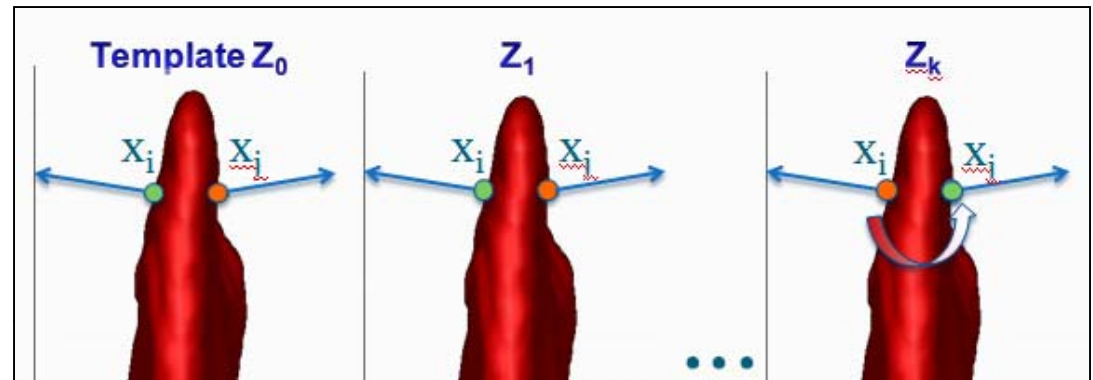


Euclidean distance very different from geodesic distance: Points do not lie in each other's tangent space



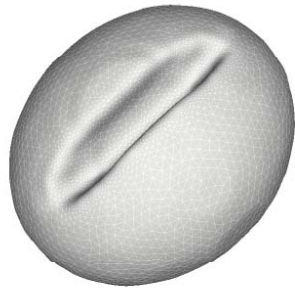
# In progress ...

- Use Geodesic instead of Euclidean distances
- Optimize ensemble entropy for consistency of the normal orientation
- Utah-UNC collaboration

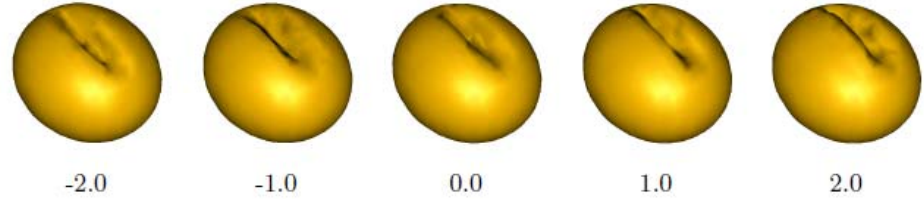




# Early results



new method



old method

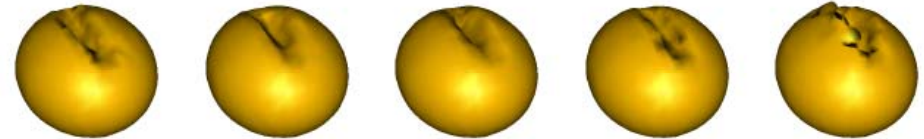


Fig. 4. Mean shape computed from the proposed method (top) and the original method (bottom), projected onto the first PCA mode, upto 2 standard deviations

DBP:  
Utah AFIB

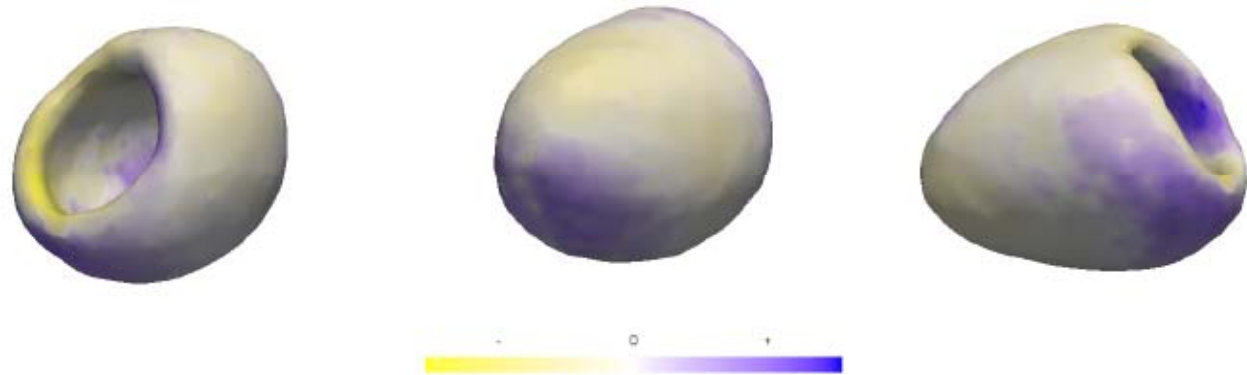
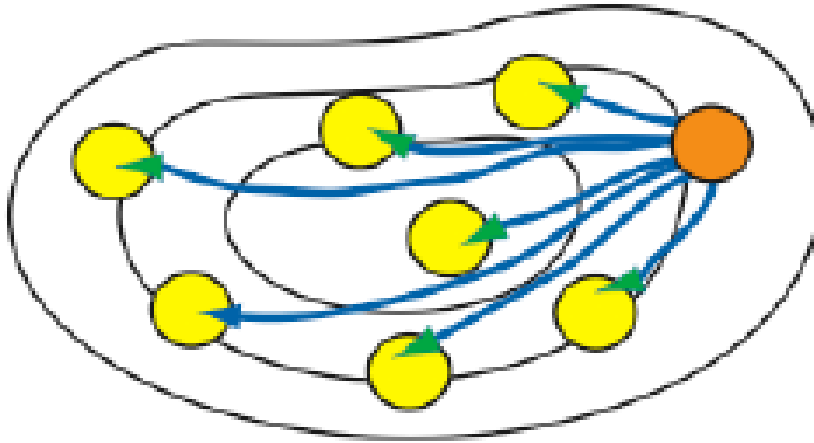


Fig. 5. Visualizing mean differences between normal and ischemic groups (blue denotes expansion and yellow denotes contraction).



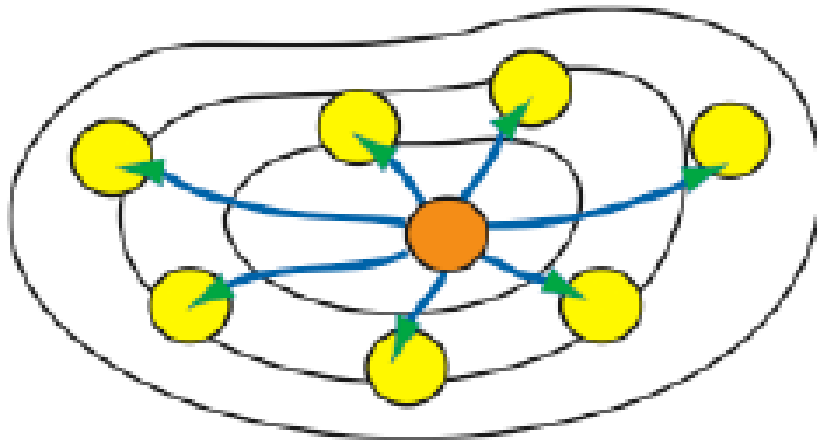
# Group-wise Registration



**Problem:** Find optimal template (“average”)

Minimize total “distance”  
between population and  
template: UNBIASED ATLAS  
BUILDING

- Joshi&Fletcher
- Gee & Avants, 2006)
- Balci, Golland, Wells  
2007





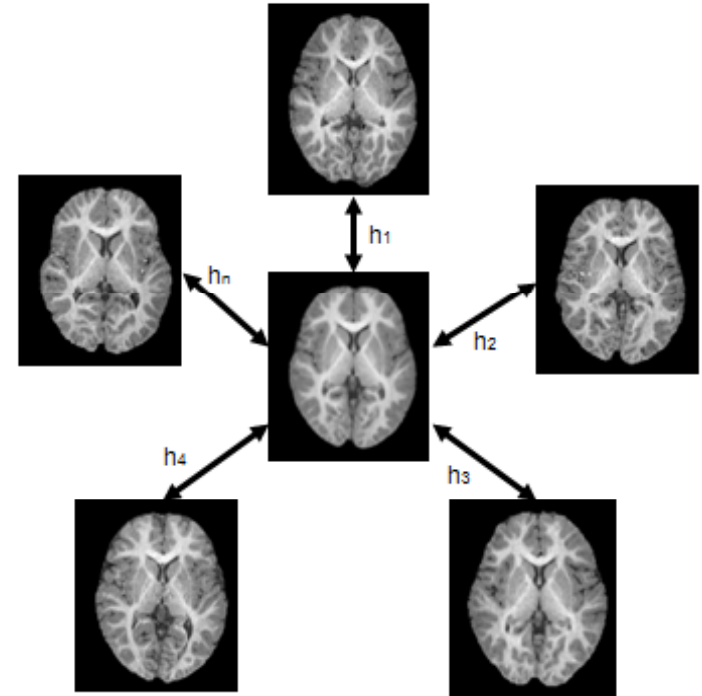


# NAMIC work in progress

- **Method:** Free-Form B-spline Deformation Model for Groupwise Registration
- **Joint alignment criterion:** Sum of pixelwise entropies:

$$f = \sum_{v=1}^V H(I(T(x_v))).$$

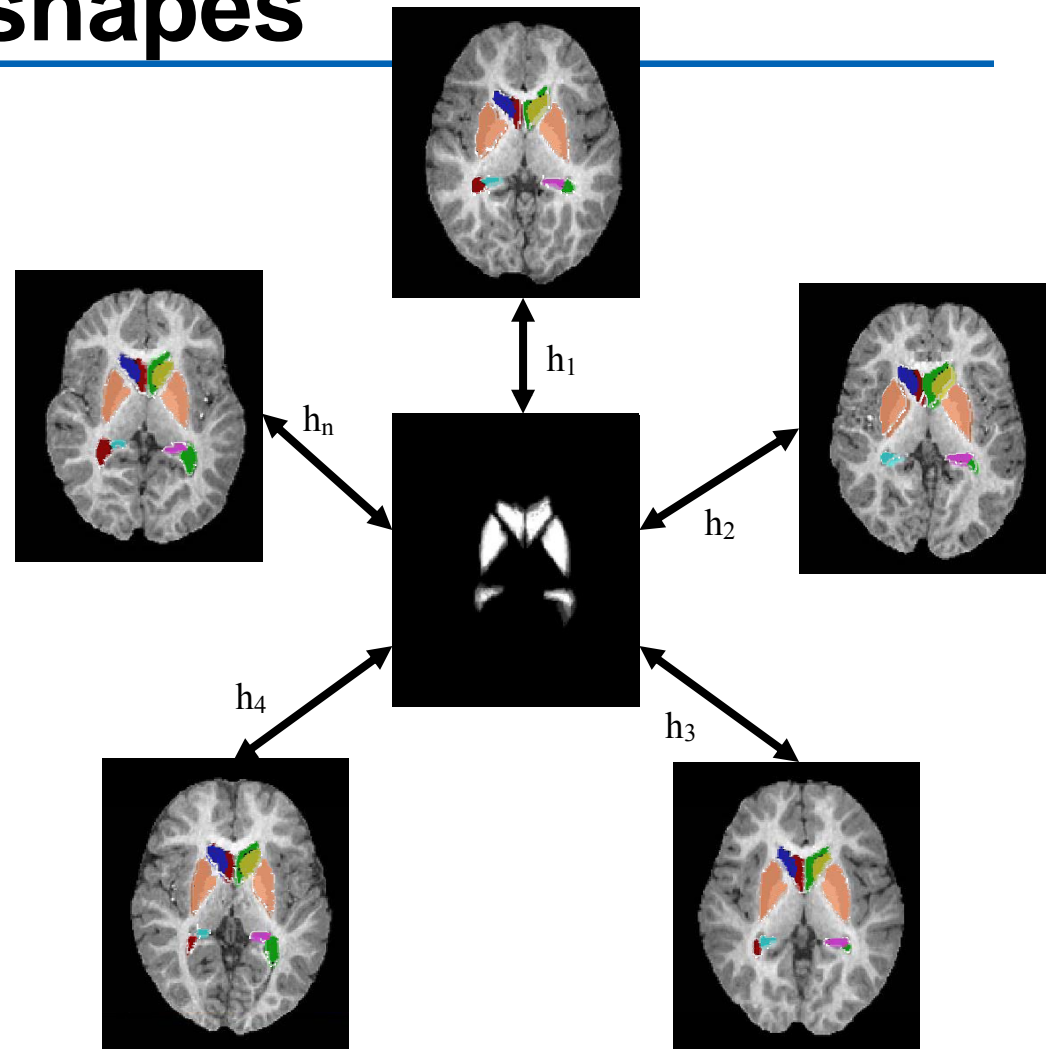
- **Result:**
  - Set of deformed images
  - Set of deformation fields  $h_i$
- **Use:** Normative atlases, establishing correspondence across subjects/time



Serdar K. Balci, Polina Golland, Martha Shenton, and William M. Wells, 2007



# Correspondences via embedded shapes



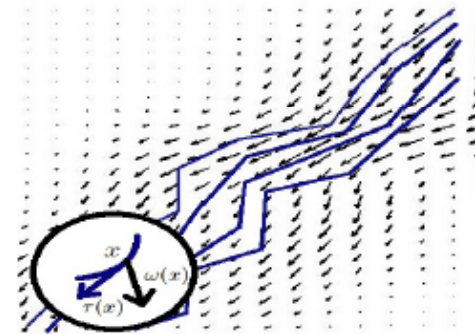


# Correspondence-free Registration

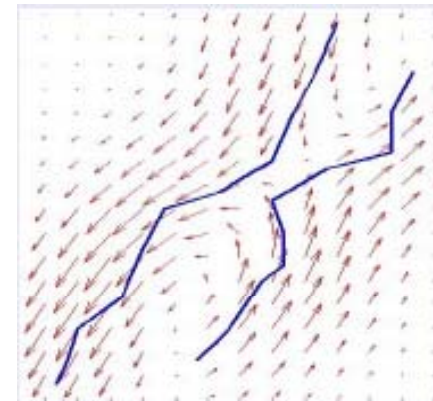
Topology and shape differences can make point-to-point correspondence hard:

- **Currents:** Objects that integrate vector fields
- **Shape:** Oriented points = Set of normals (tangents)
- **Distance** between curves:

$$d(L_1, L_2)^2 = \int_{L_1} \omega_1(x)^t \tau_1(x) dx + \int_{L_2} \omega_2(x)^t \tau_2(x) dx - \int_{L_1} \omega_2(x)^t \tau_1(x) dx - \int_{L_2} \omega_1(x)^t \tau_2(x) dx$$



$$L(\omega) = \sum_{i=1 \dots A} \int_{L_i} \omega(x)^t \tau(x) d\lambda(x)$$

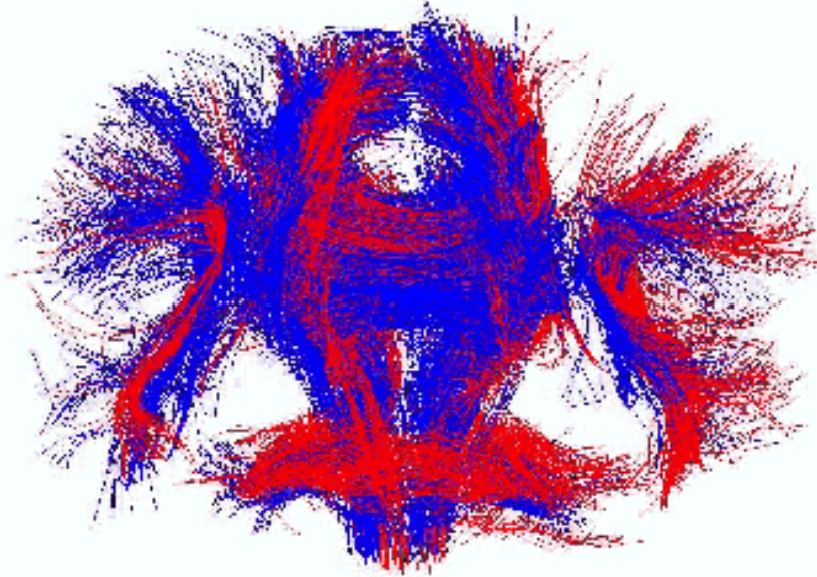


[Glaunes2004] Glaunes, J., Trounev, A., Younes, L. Diffeomorphic matching of distributions: a new approach, ... CVPR 2004.

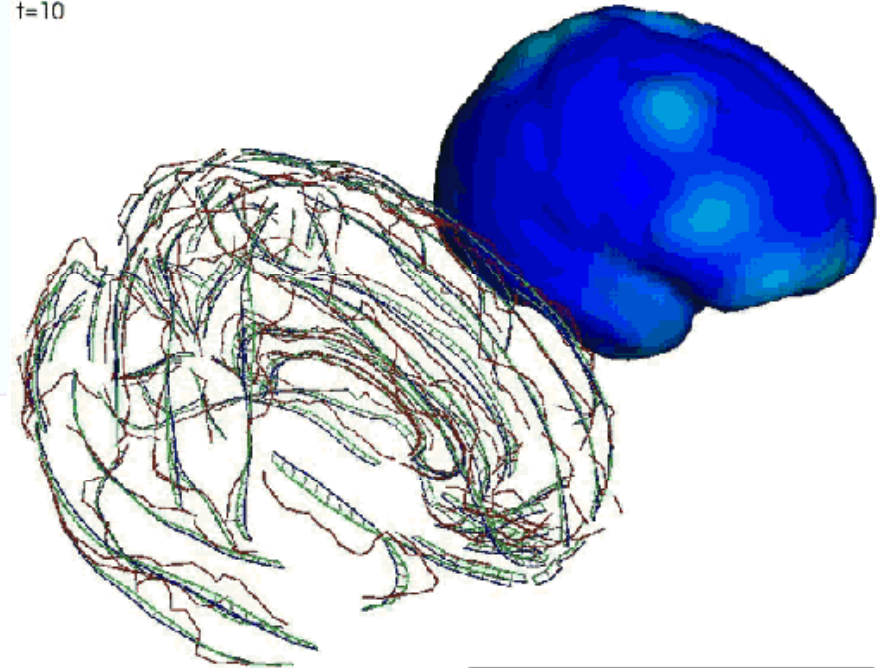
[Durrleman2008] S. Durrleman, X. Pennec, A. Trounev, P. Thompson, N. Ayache, Inferring Brain Variability from Diffeomorphic Deformations of Currents: an integrative approach, Medical Image Analysis 2008



# Relevance to NAMIC: Registration in presence of large deformations



t=10



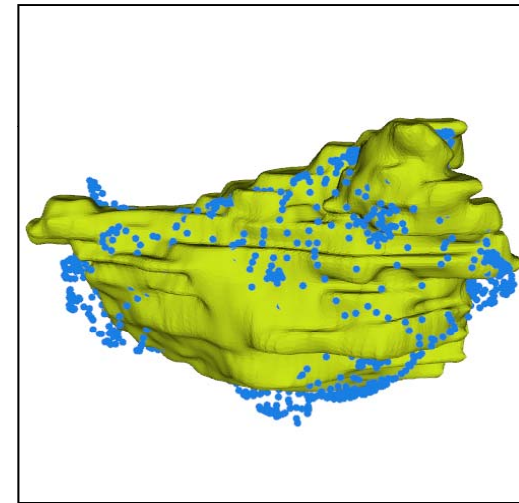
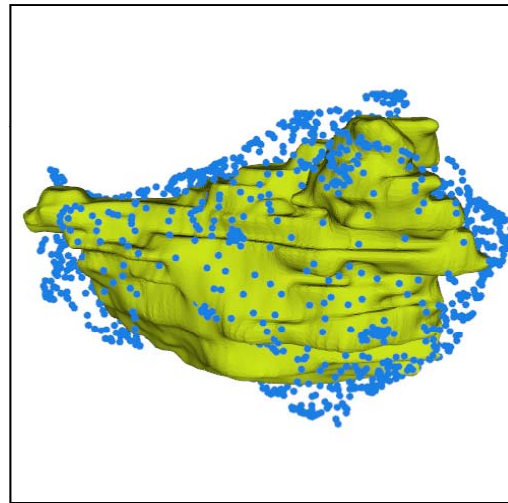
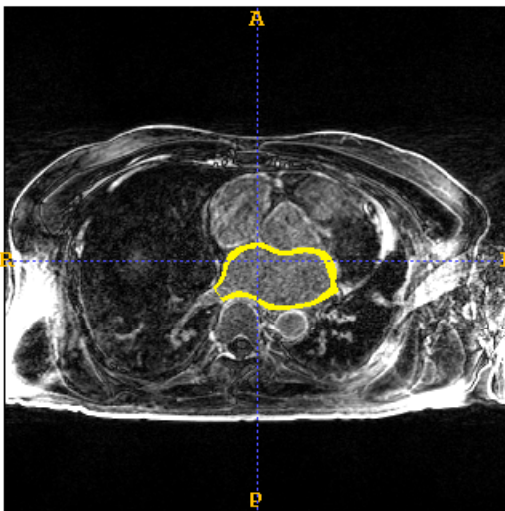
Registration without explicit point-to-point correspondence.

Material courtesy of Stanley Durrleman



# Correspondence-free mapping

**Problem:** Nonlinear mapping of point sets with different resolutions.

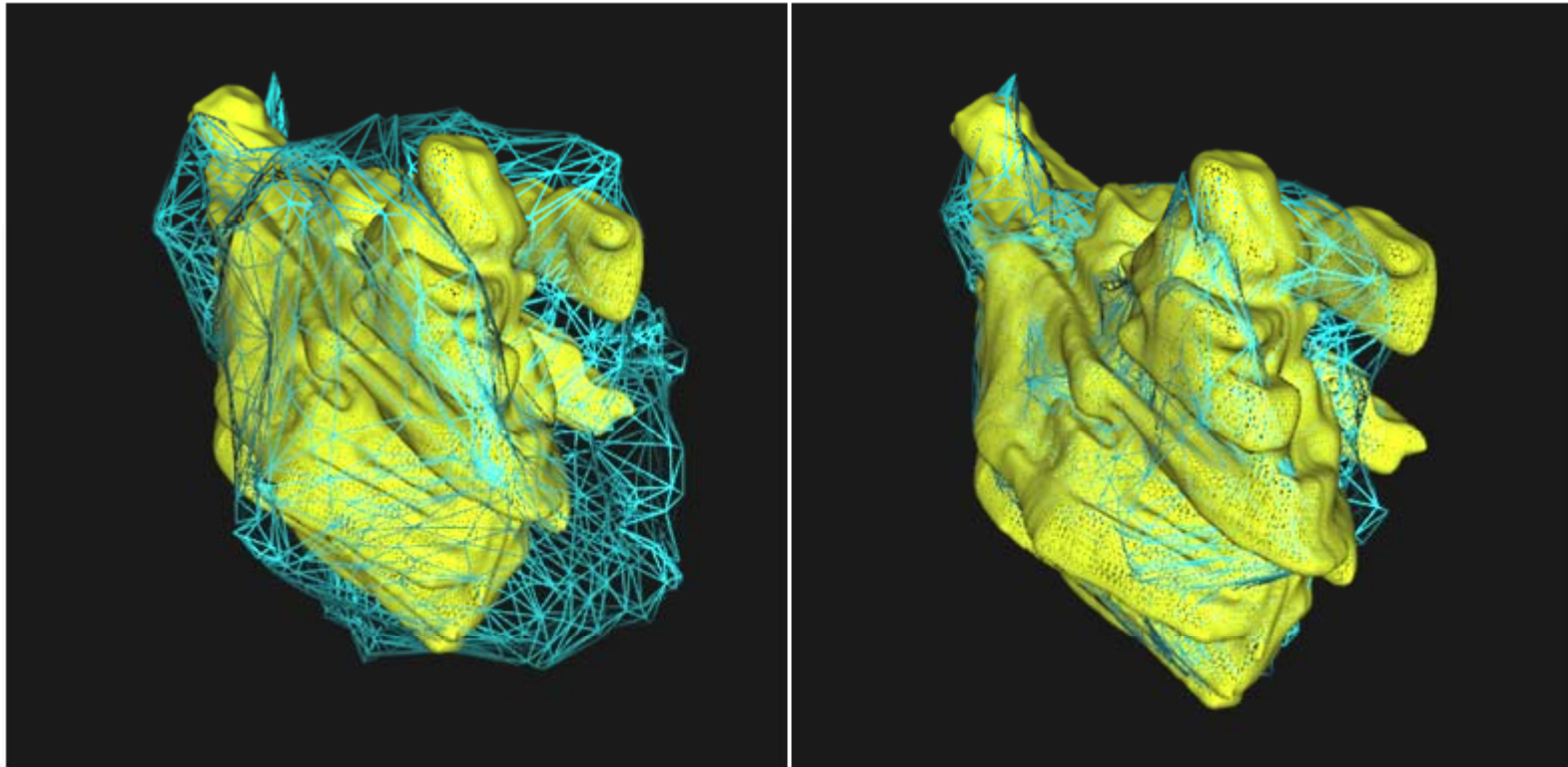


Yellow: high resolution surface from MRI segmentation (32172 points). Blue: low resolution surface from catheter tracking (1803 points). Left: Initial manual alignment. Right: Automatic alignment using currents measure with a combination of affine and elastic transformations.



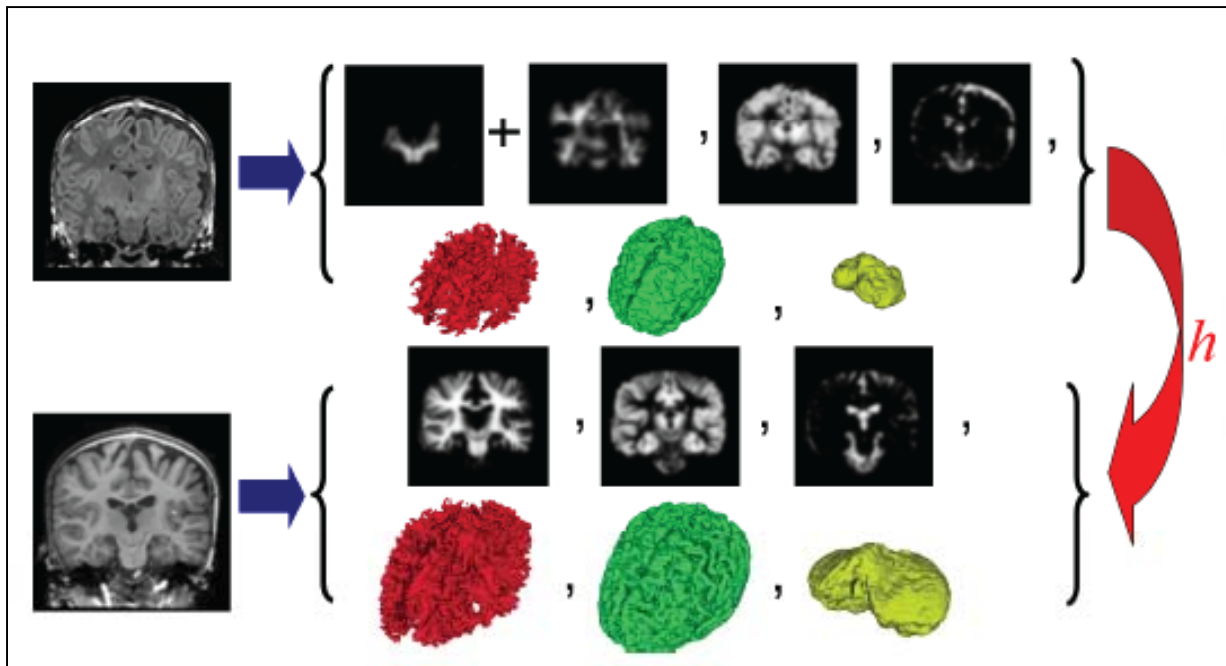
# Correspondence-free mapping

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# Registration via Combined Probabilistic and Geometric Descriptors



Deformable image registration in the presence of considerable contrast differences and large-scale size and shape changes represents a significant challenge for image registration → **Use Appearance and Geometric Features**

Linh Ha, Marcel Prastawa, Guido Gerig, John H. Gilmore, Claudio T. Silva, and Sarang Joshi. *Image Registration Driven by ...*, MICCAI 2010



# Conclusions

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- NAMIC R&D has to tackle challenging scientific problems w.r.t. geometric correspondence and registration:
  - Longitudinal/serial data presenting significant changes
  - Complex expression of pathology: New objects, change of topology
  - Multi-modal longitudinal registration
- Core methods are not yet readily available, no off-the-shelf solutions
- Very promising quick start on DBP problems
- Strong Core1a/b team effort towards short-/mid- and long-term solutions, driven by needs of DBPs and NAMIC-associated projects