



NCIGT Computation Core

**NIH and NCIGT Joint Workshop on
Clinical Image-Guided Therapy:
Opportunities and Needs**

March 10-11, 2008

Rockville, Maryland

William (Sandy) Wells





Computation Core

- Slicer Engineering
- High Performance Computation (HPC)
 - Interventional nonrigid registration
- Spatial Neuroinformatics (SNI)
 - fMRI for neurosurgery
- Endoscopic Navigation
- Neurosurgical Image Database



- **Is Part of: NA-MIC Kit** - *Software and Methodologies for Medical Image Computing*
 - NAMIC: an NCBC: National Alliance for Medical Image Computing
 - Facilitate Research
 - Promote Interoperability
- Stable, Cross-Platform Run Time Environment
 - Full set of core features
- Flexible Module Architecture
 - Plug-ins added as needed

Fully Open, Interoperable Components

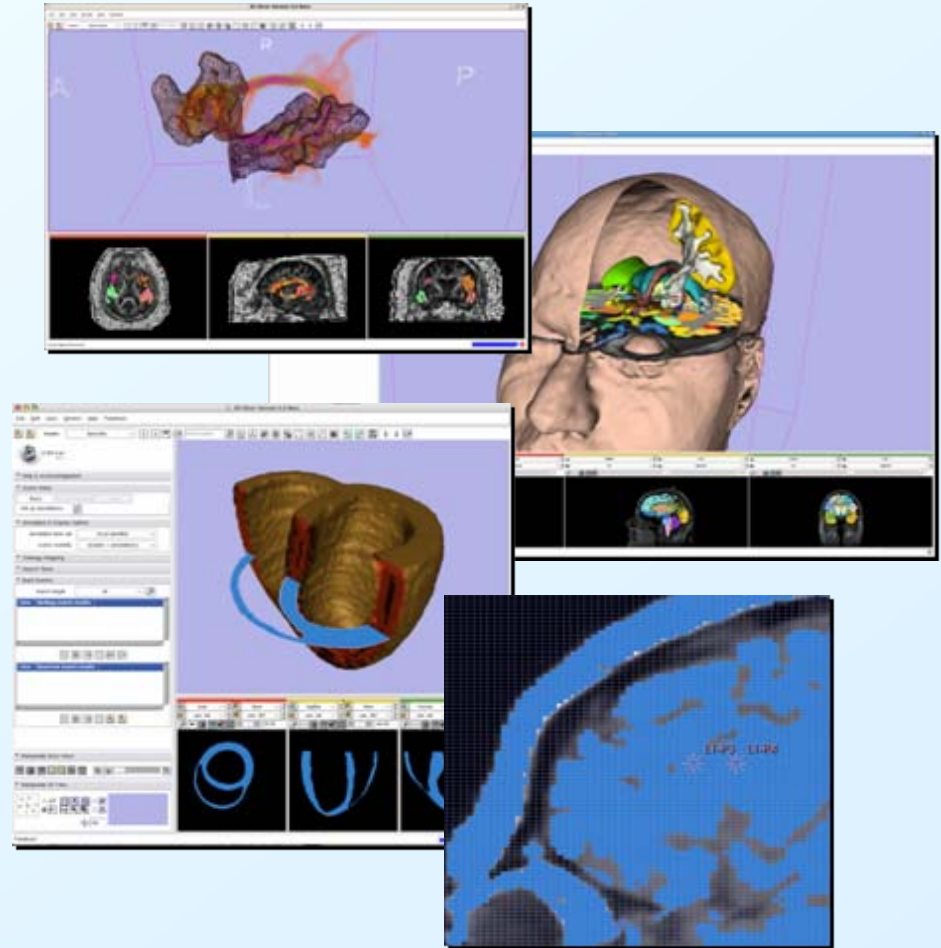
- End User Application
 - 3D Slicer
- Image Analysis, Visualization, and GUI libraries
 - ITK, VTK, KWWidgets
- Large Scale Data Processing Tools
 - Batchmake, XNAT, BIRN GRID tools
- Software Engineering Tools
 - CMake, Dart, CTest, CPack



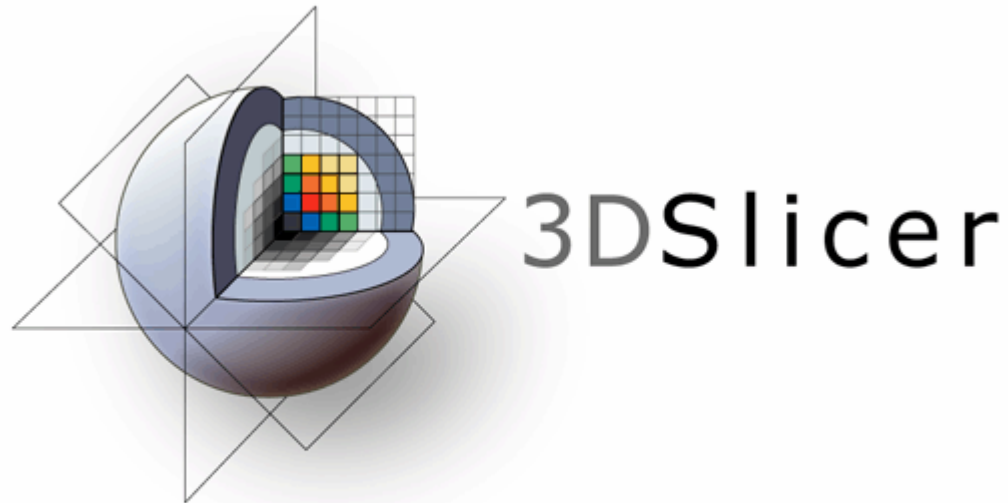
<http://www.na-mic.org/Wiki/index.php/SoftwareInventory>



- XML-Based MRML File Stores Scene Description
 - Volumes (Images, Label Maps)
 - Models
 - Hierarchical Affine Transforms
 - Scene Data (Cameras, Colors, Fiducials, etc)
 - Undo/Redo, Scene Snapshots
- Careful Attention to Coordinate Systems
 - Scalar Images
 - Diffusion Images
 - Time Series (fMRI)
 - Visualization

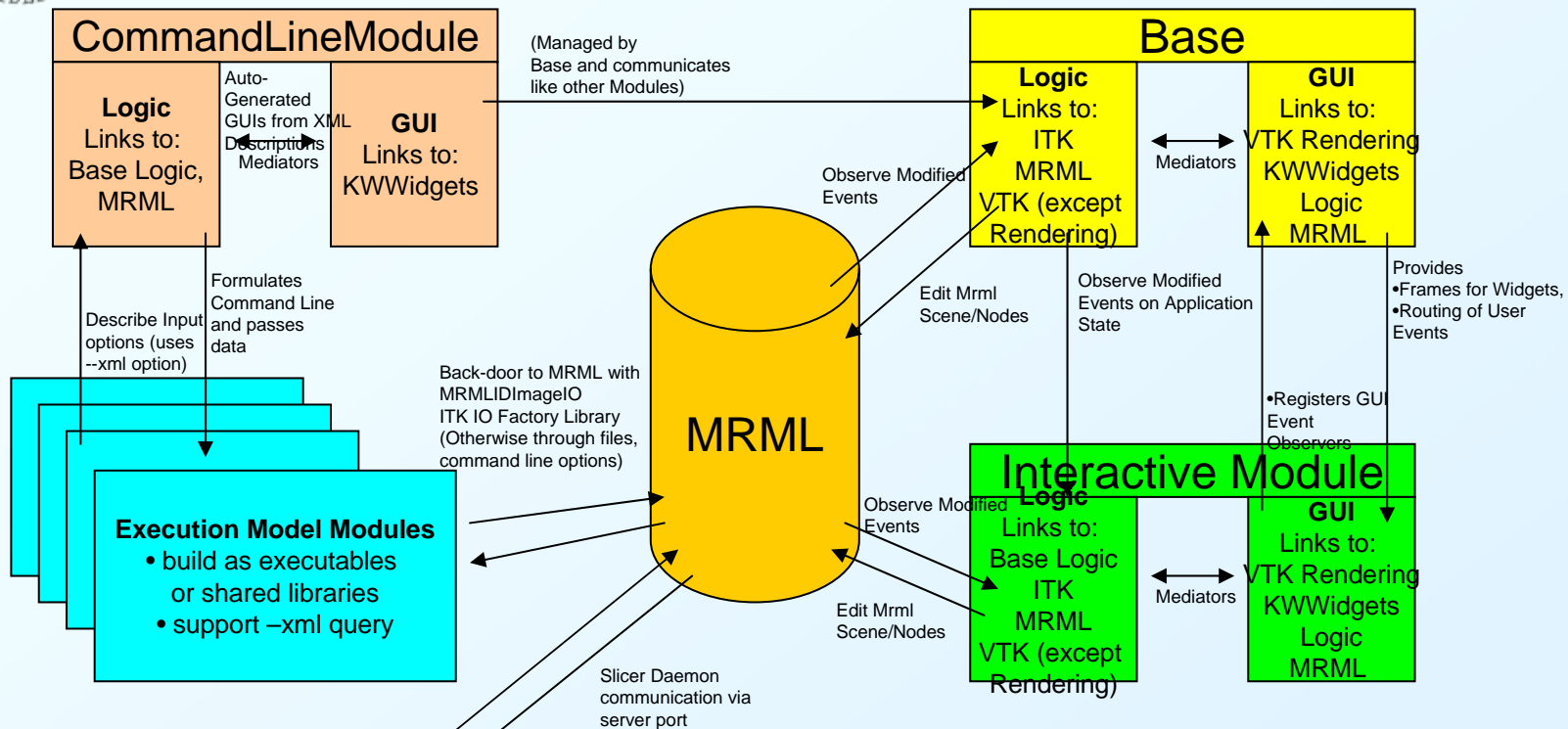


Slicer3 Architecture



Supported by NA-MIC, NAC, BIRN, NCIGT and the Slicer Community.
See <http://www.slicer.org> for details.

Slicer 3 Architecture Diagram (updated 2007-01-09)



Notes:

- All classes in the Logic directory should be able to run 'headless' without OpenGL or window system for scripting and testing
- Base Logic and GUI contain transient application state (cursor location, focus, mrrml scene connection...)
- Persistent and Undoable state in MRML Nodes
- Interactive Modules are ones which interact with the VTK scene and/or User events
- Interactive Modules interact with 3D scene by creating objects in MRML scene (not by direct manipulation of the Renderer)
- Logic classes encapsulate and manage internal vtk/itk pipelines and provide helper routines to create/manage nodes
- GUI classes are implemented as KWWidget subclasses
- Each Logic class defines Get/Set methods for internal state and Modified Events that GUI classes can Observe
- Code in Base implements "first order" Node types (Volumes, Models, Transforms, Fiducials, Colors, etc).
- Code in Modules provides application-specific extensions



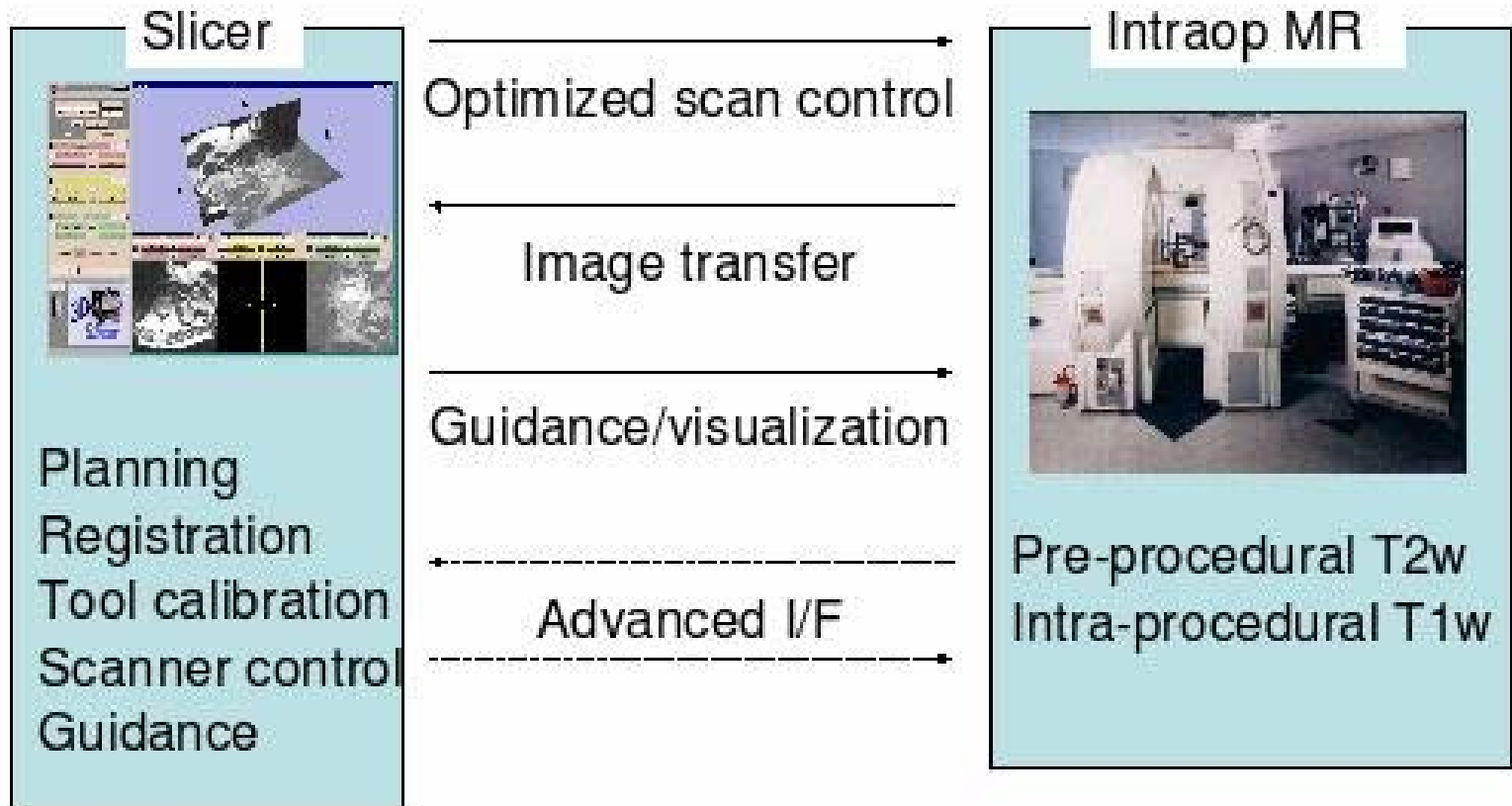


NCIGT: Slicer Engineering

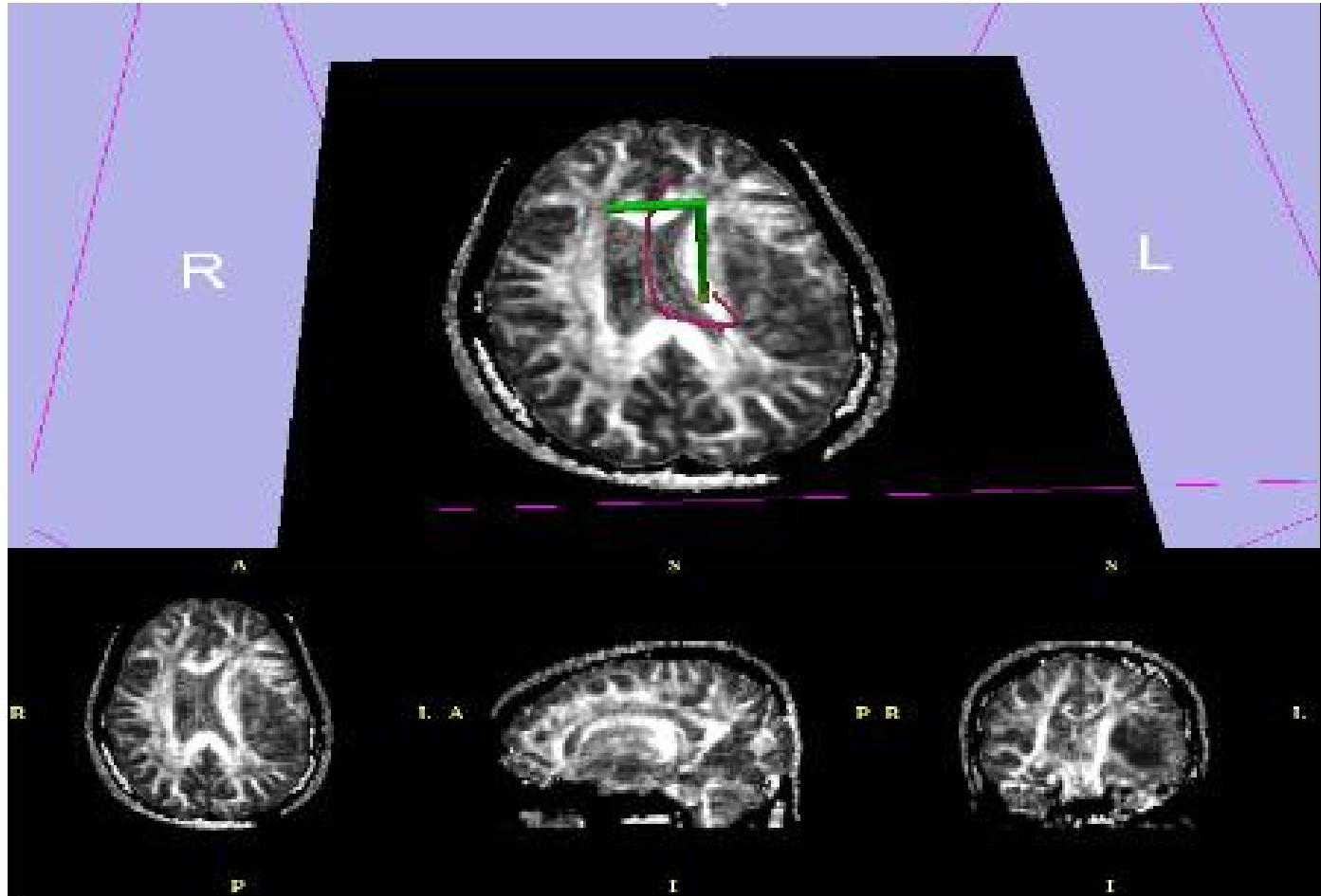
- Slicer 2.6
 - Intra op display DTI fMRI
 - GUI for non-rigid registration
 - Open tracker integration
 - IGT modules
 - MRProstate Care
 - Tractography for neurosurgery
 - NeuroNav module
 - 120 clinical applications
- Slicer 3.0: integrate IGSTK



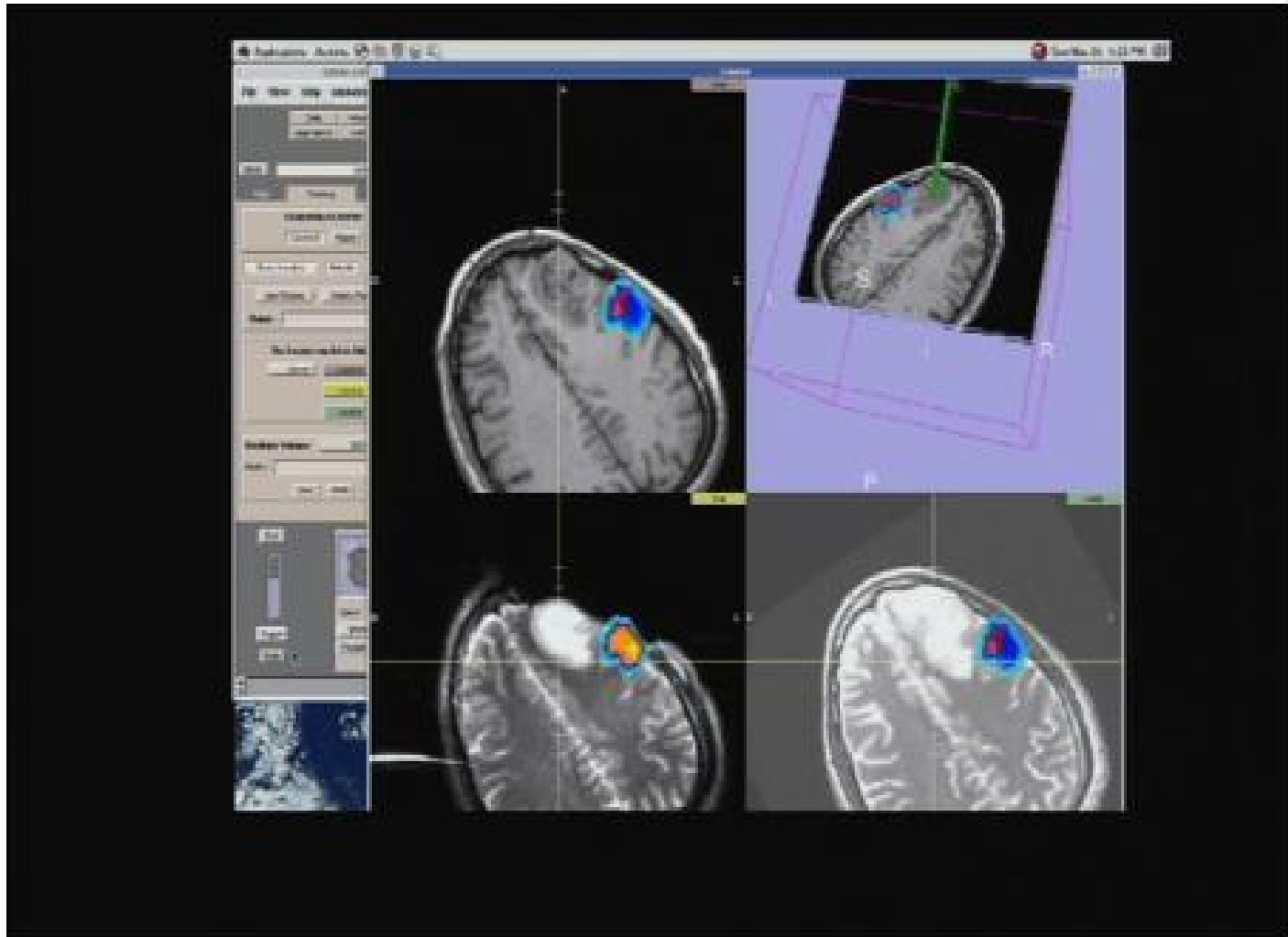
Prostate biopsy with 3D Slicer



Tractography within neuro navigation



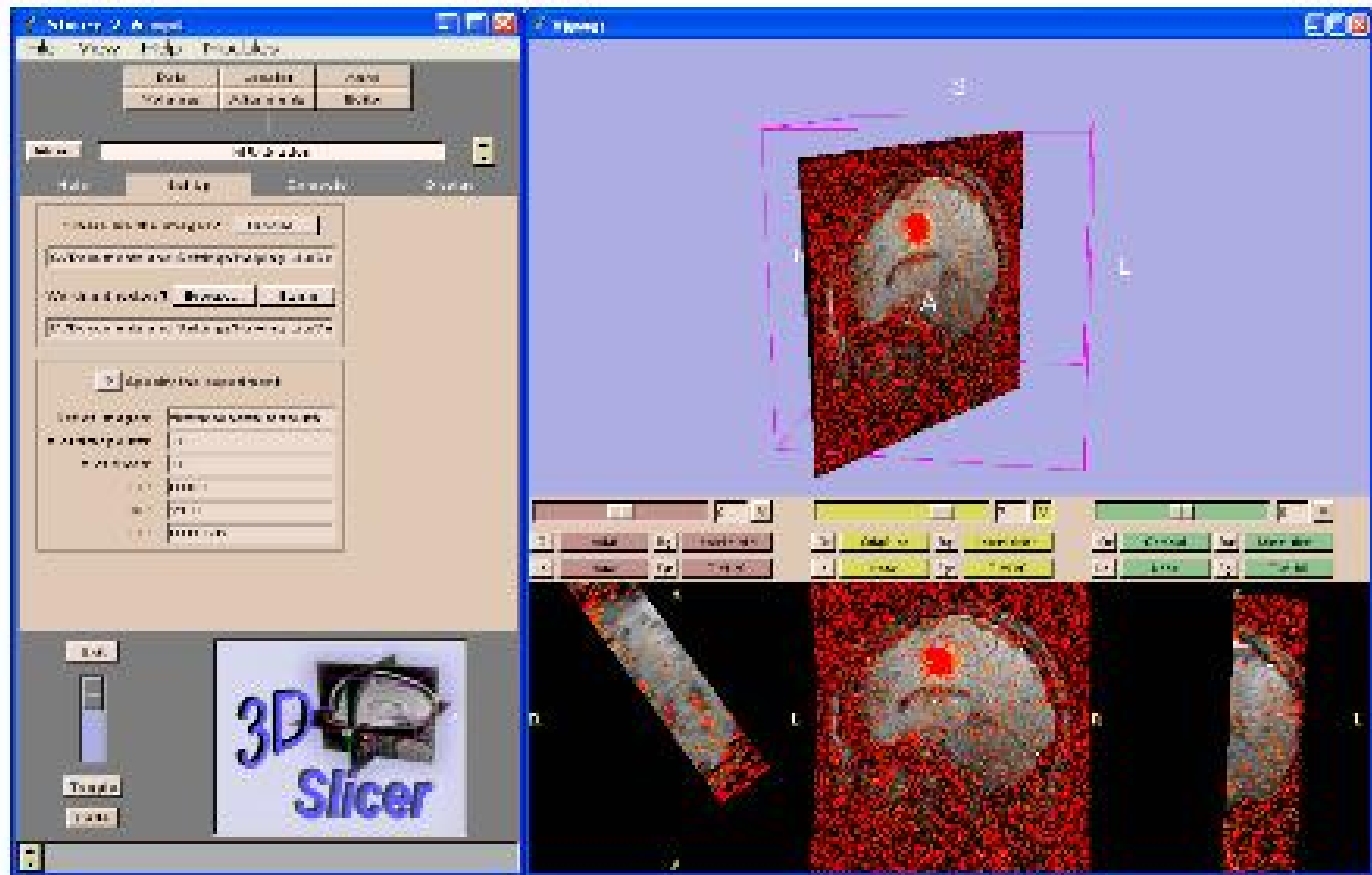
Neurosurgery with 3D Slicer



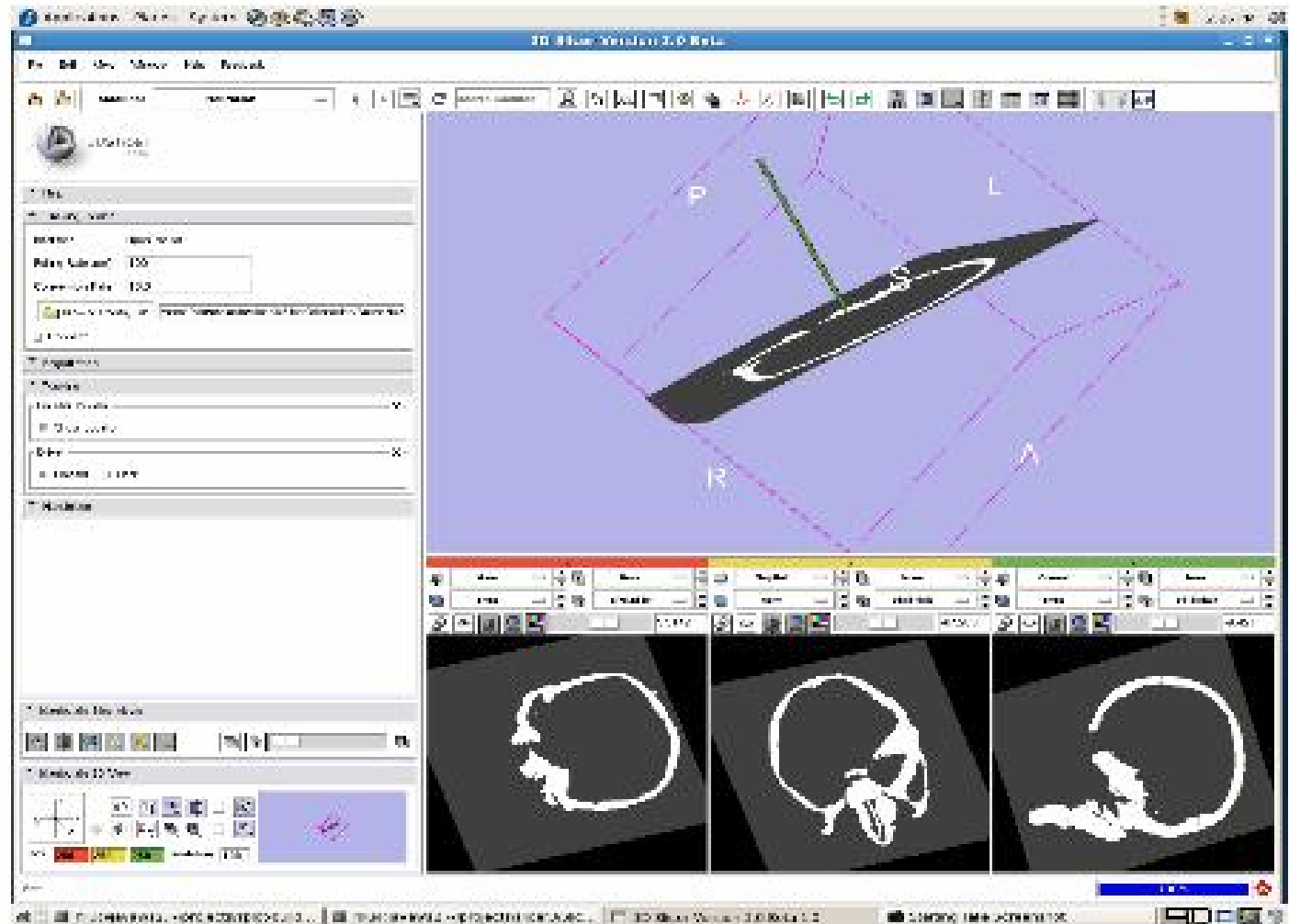
MRProstateCare module in Slicer2.6 for prostate biopsy



MR Ablation module in Slicer2.6 for laser ablation



NeuroNav module in Slicer3





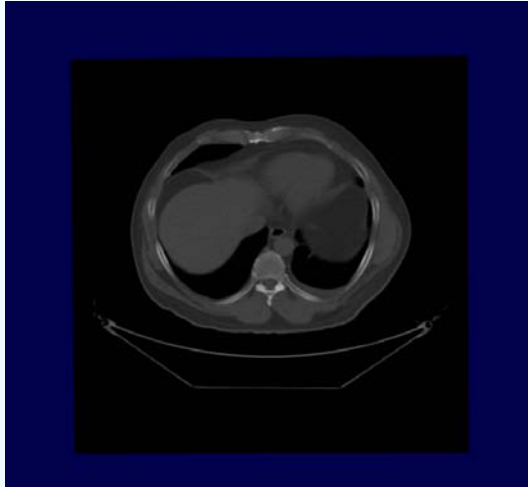
High Performance Computing

- Grid computing w/ William and Mary's
- block matching, visual feedback to surgeon
- Improved targeting IG ablation

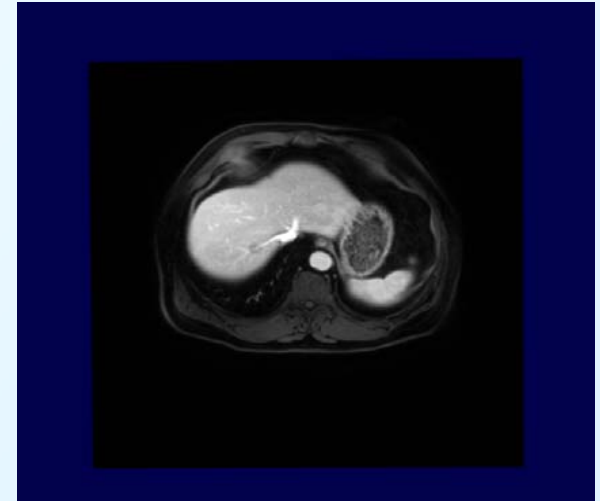


Pre-procedural images: PET/CT and MRI – aligned using non-rigid registration

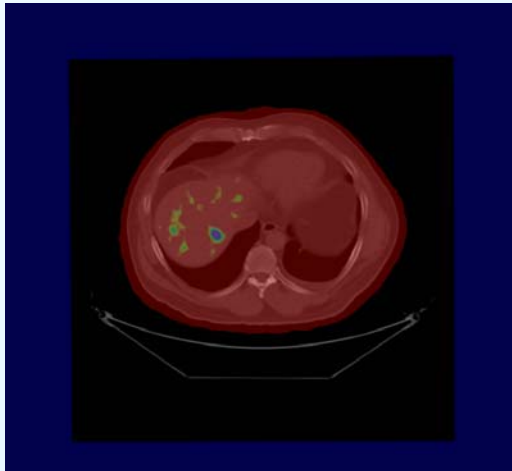
CT of patient with a liver tumor located adjacent to the diaphragm (lesion not visible on CT)



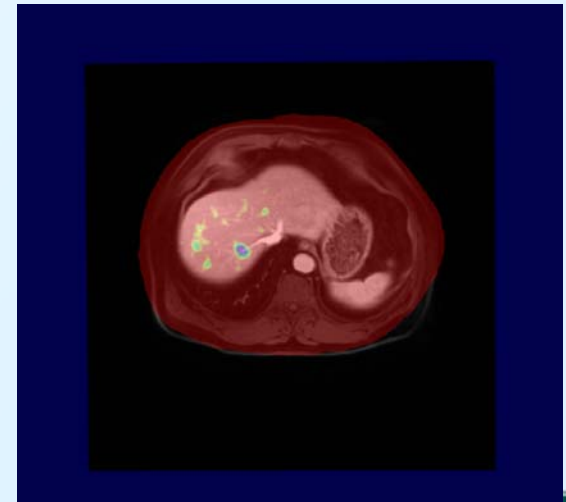
Pre-procedural axial MRI at the same level as the CT



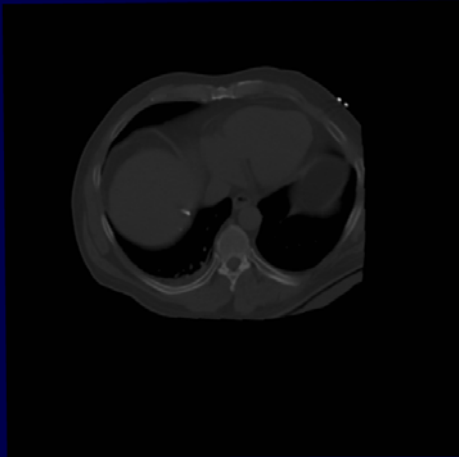
PET registered with CT (the tumor is clearly depicted on PET)



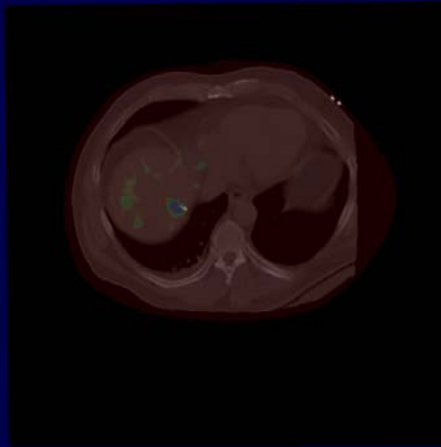
PET registered with MRI, using the same transformation field obtained from MRI to CT registration



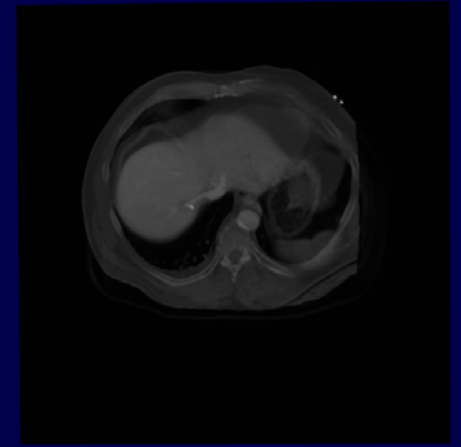
Intra-procedural CT images during targeting registered with pre-procedural PET/CT and MRI



Intra-procedural CT
during targeting (tumor
not visible)



Enhanced tumor visulation
obtained by aligning intra-
procedural CT with the pre-
procedural PET



Intra-procedural CT during
targeting, registered with
pre-procedural MRI for
enhanced tumor
visualization

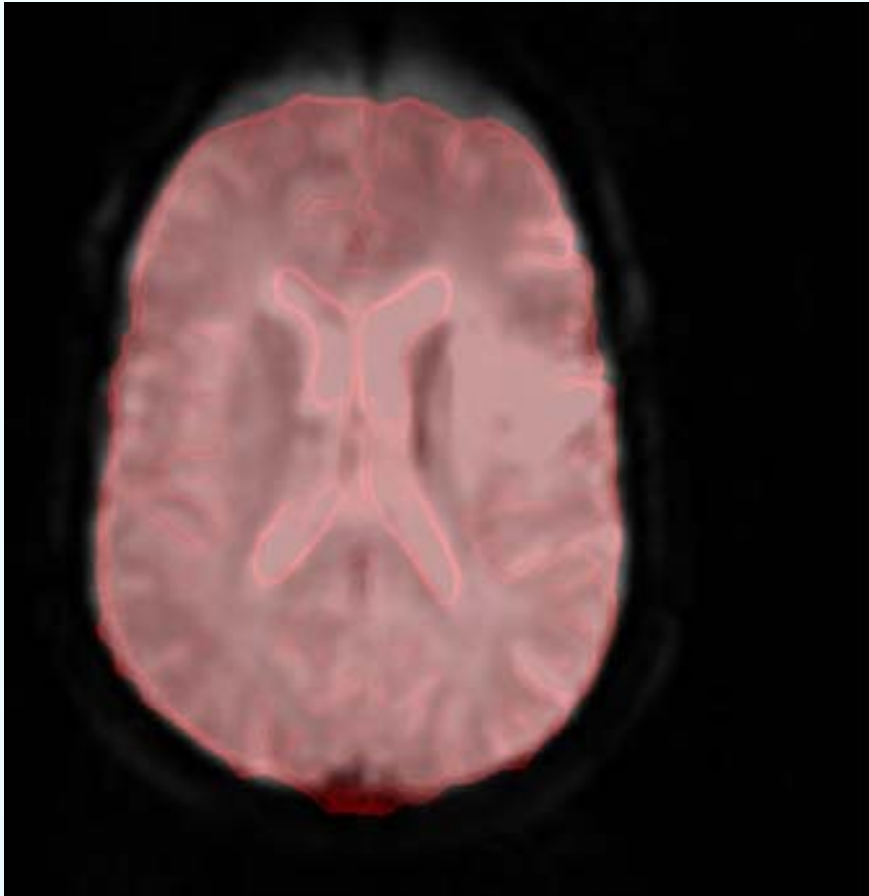


Spatial Neuroinformatics

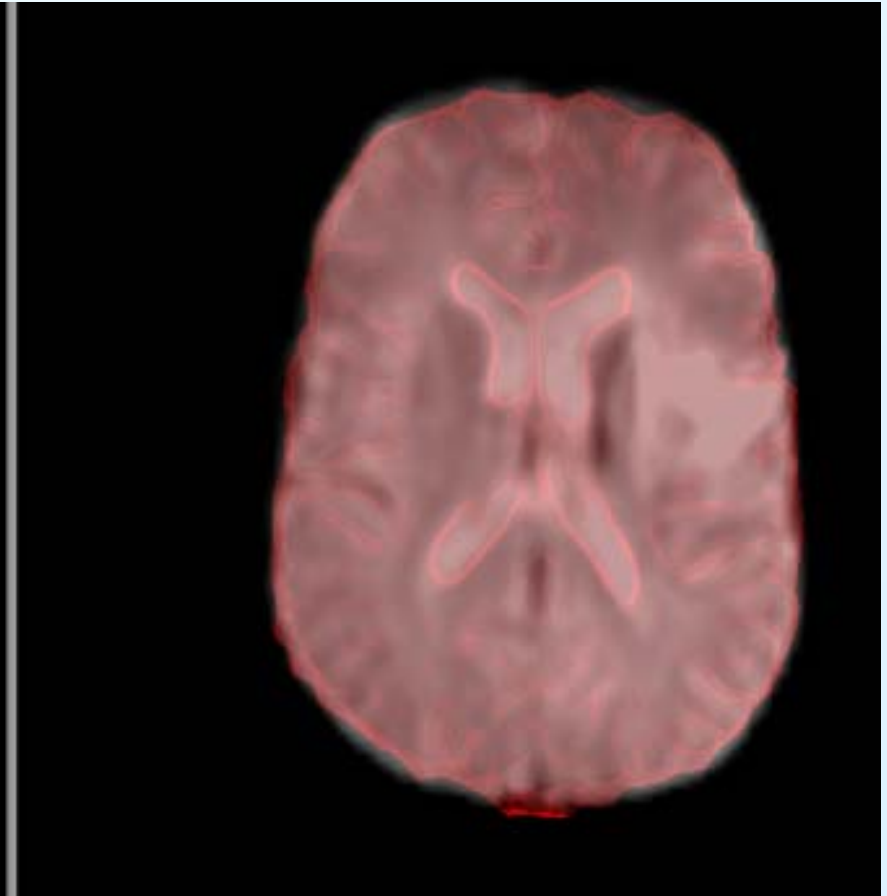
- EPI dewarping: methodology, initial experiments
- EPI distortion
 - How bad is it
 - How good is “field map” solution?
 - Develop “MRI-based” correction



EPI / MRI agreement



Without fieldmap correction



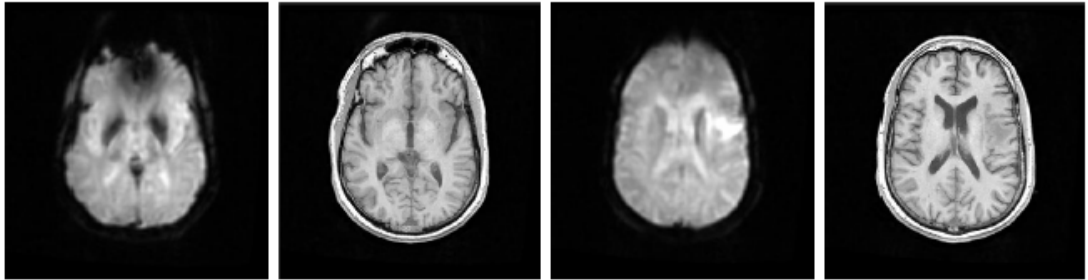
With FSL fieldmap correction

EPI registration

(e) (f): rigid registration
Without dewarping

(g) (h): affine registration
Without dewarping

(i) (j): dewarping with fieldmap

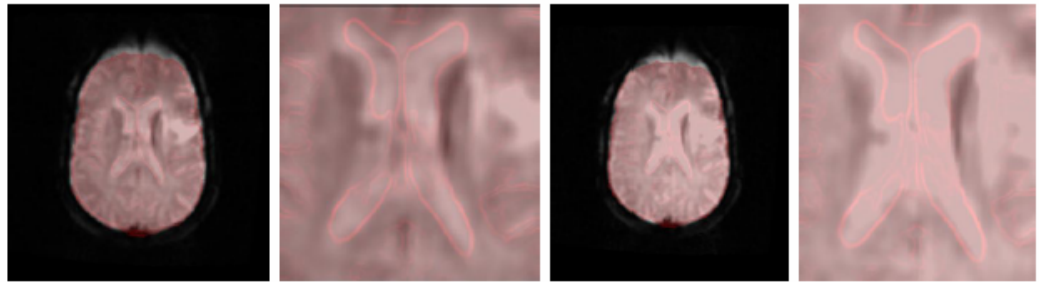


(a)

(b)

(c)

(d)

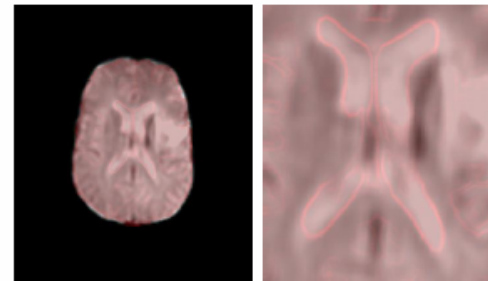


(e)

(f)

(g)

(h)



(i)

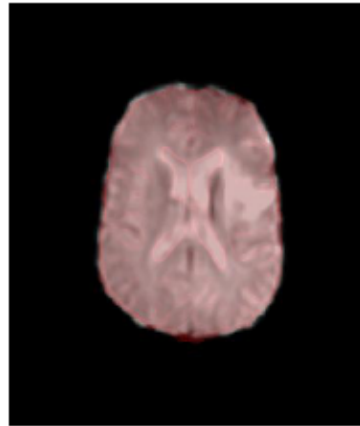
(j)

Recent Results

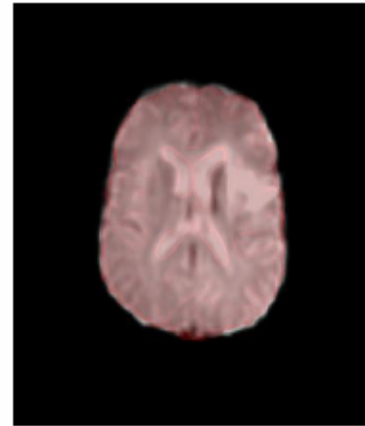
(e) (g): dewarping with
Acquired fieldmap

(f) (h): dewarping with
Fieldmap predicted
Structural MRI

Clare Poynton MICCAI
submission



(e)



(f)



(g)



(h)



Tracked (Image Registered) ENDOSCOPY

NCIGT March, 2008



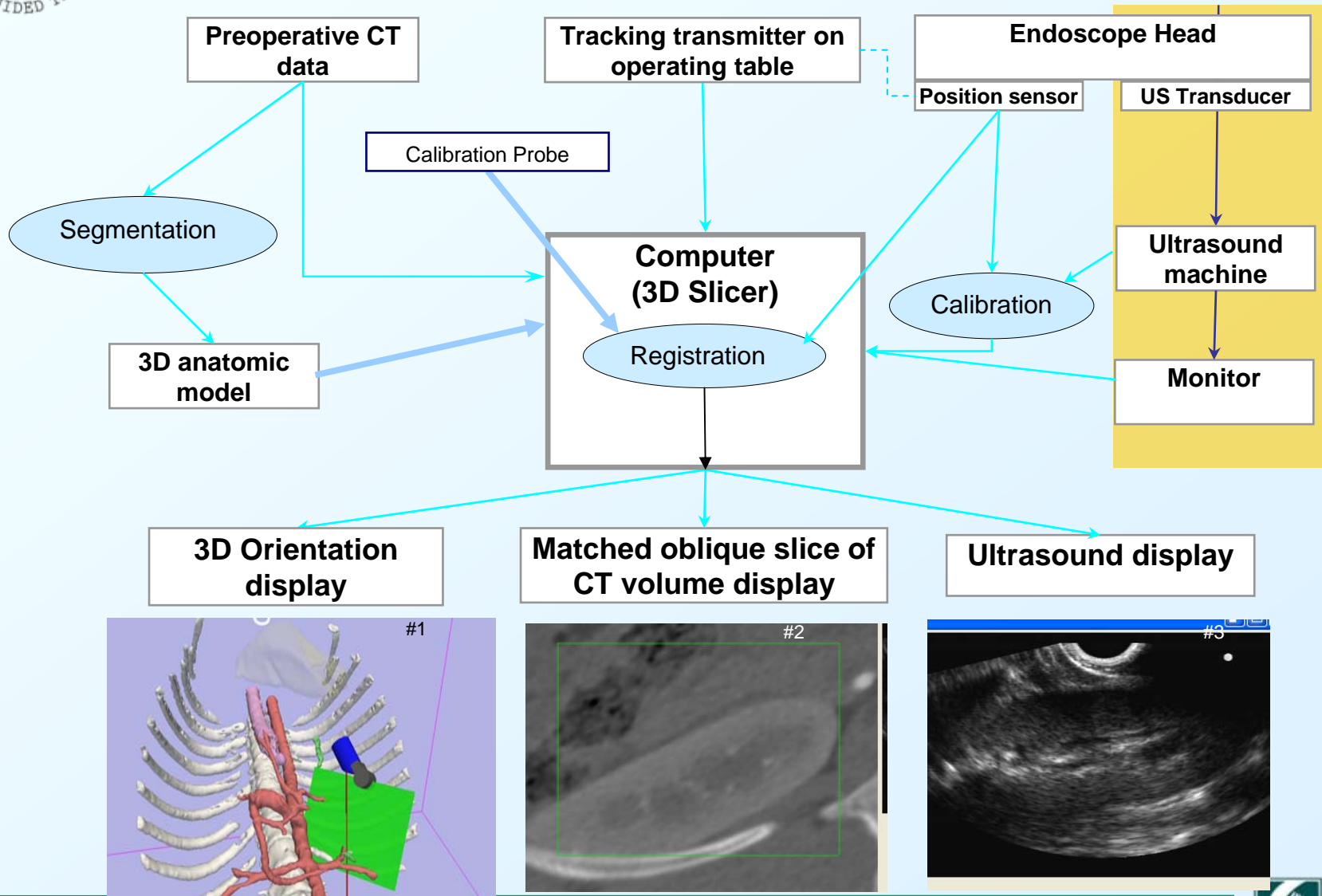


Image Registered Endoscopy

- Overall Goal: Improve endoscopic imaging by integrating with other pre-operative and intra-operative imaging modalities
-
- The increasing quality and use of screening and diagnostic scans (CT, MRI, PET,...) will increase demand for minimally invasive biopsy and intervention
 - Initial work is focused on Endoscopic Ultrasound (EUS) where image registration may have the most impact because the image plane position may be difficult to determine. Today, these techniques have not maximally adopted by gastroenterologists and surgeons due to:
 - Long learning curve
 - Lack of confidence in ultrasound interpretation
 - We hypothesize that the display of the position and orientation of the ultrasound probe in anatomic context and display of CT (or MR) “Reference Images” will improve the accuracy and confidence of physician operators.

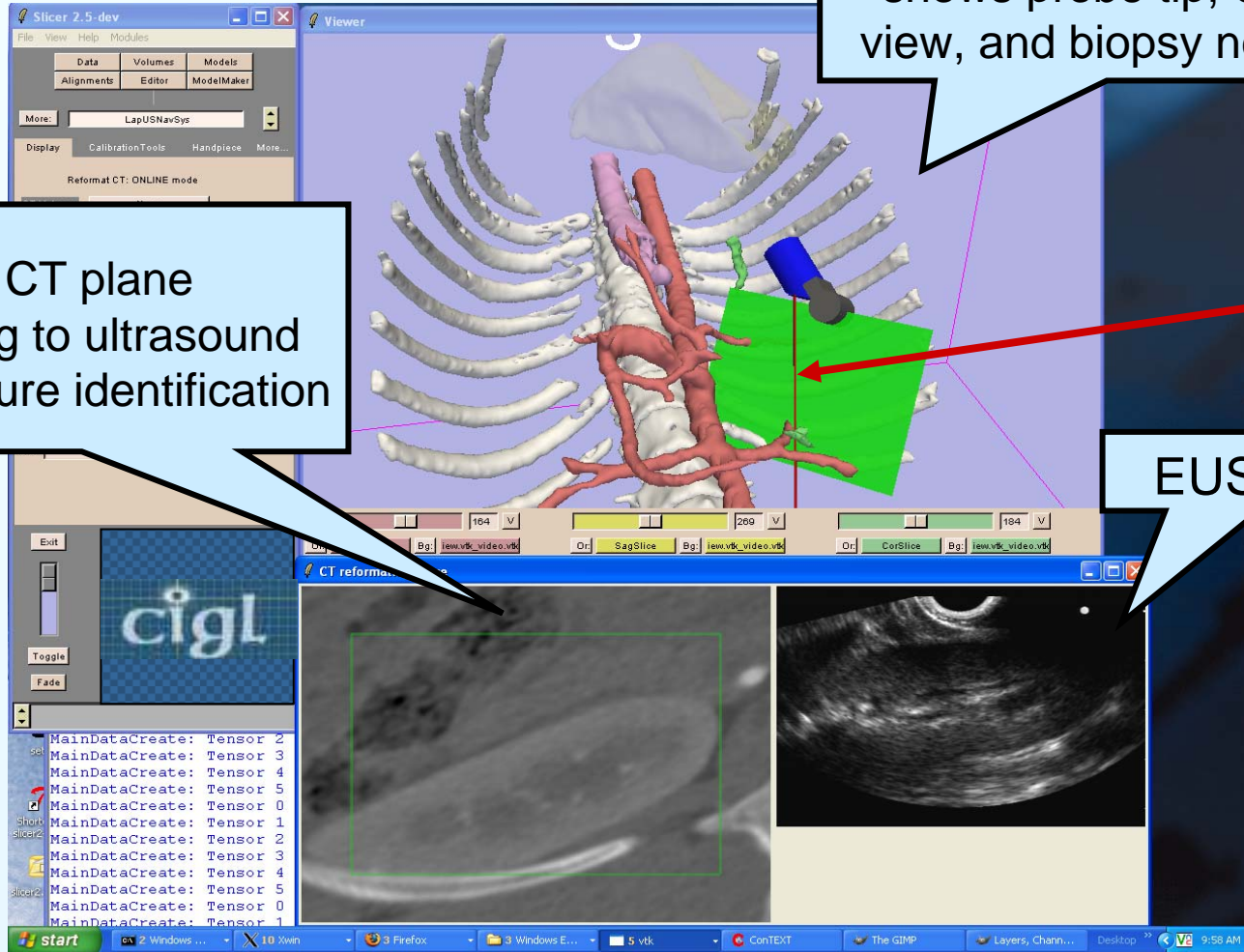


System Data Flows



IRGUS Display

Segmented 3D CT for Orientation of probe. Icon shows probe tip, US field of view, and biopsy needle track



Oblique CT plane corresponding to ultrasound image for feature identification

Needle Track

EUS image



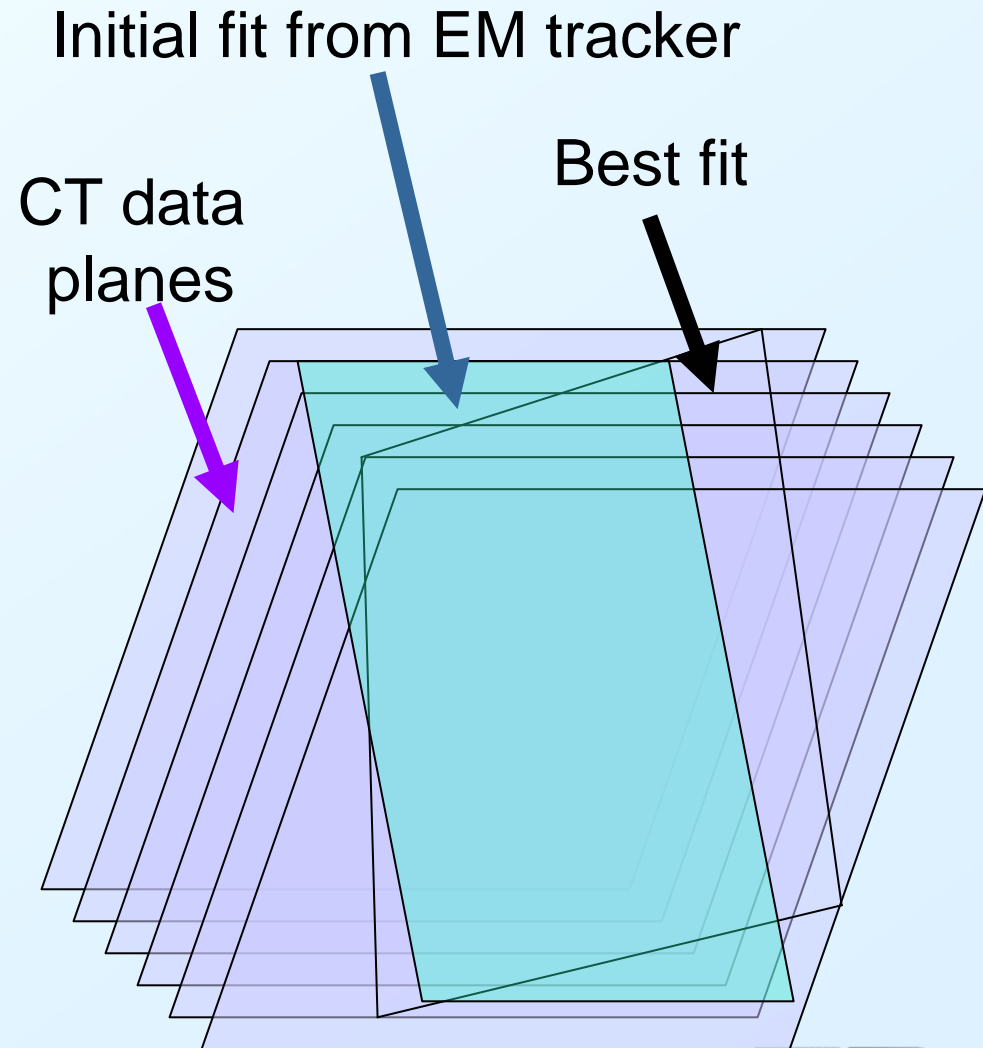
2008: Focus on Human Studies

- Validate registration in OR/endo suite setting
 - Lap pancreas surgery at Dalhousie
- Finish patient pose study (BWH)
 - What compensation is required when patients are lying on their side?
- Open pancreas surgery at MGH
- Gastrosopic Ultrasound/Endoscopy at BWH
- Technical development
 - Staged Registration (ANU Canberra)
 - Ultrasound image interpretation
 - C-PASS kinematics analysis for validation



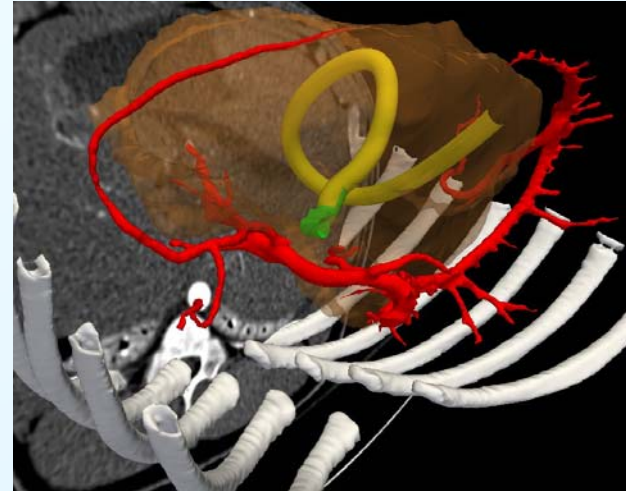
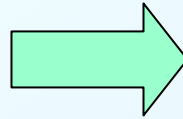
Robust Real-time Tracking

- Initial fit from registered electromagnetic tracker
- Use image content comparisons to improve fit
 - Vascular structures
 - 2D-2D comparisons
 - 3D-3D comparisons

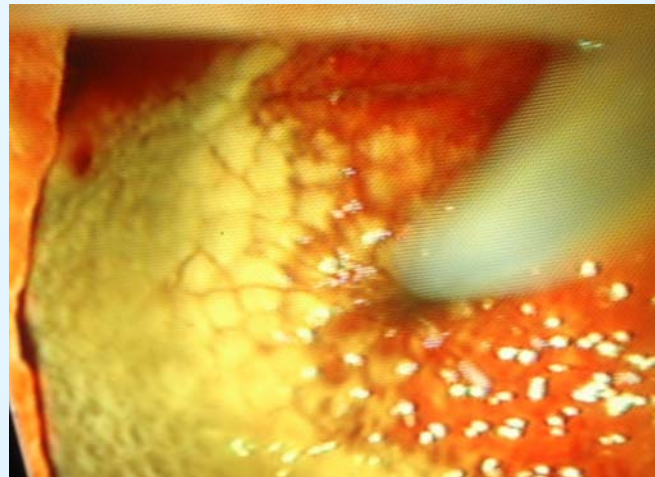
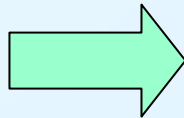


IRGUS For Gastric Access NOTES (IRGA)

- Show location of scope tip, shape of scope body
- Support interpretation of GUS image
- Mis-registration less than 5 mm
- Publications:
 - MMVR, CAS
- On hold for first human tests of IRLUS & IRGUS



**First Image Registered
Gastric Access (IRGA)
(porcine model)**





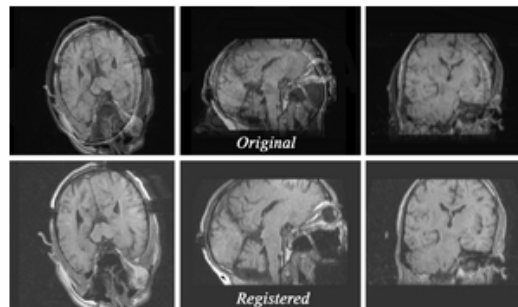
Neurosurgical Image Database

- Organize large retrospective collection of neurosurgical image data (with MRT)
- XNAT based: work in progress
- Neculai Archip, Steven Haker, Ion Florin-Talos



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Title: Volumetric Non-Rigid Registration for MRI-Guided Brain Tumor Surgery



Authors: [Ion-Florin Talos](#), [Neculai Archip](#)

Institution: Surgical Planning Laboratory, Harvard Medical School and Brigham and Women's Hospital, Boston, MA, USA.

Publisher: SPL 2007

Publication Date: Aug-2007

Citation: SPL brain tumor resection image dataset, Aug 2007

Appears in Collections: [SPL](#), [NCIGT](#), [Download Data](#), [NAC](#)

Abstract: The accuracy of neurosurgical navigation systems is seriously compromised by brain shift, i.e. changes in the spatial position of the lesion and surrounding brain tissue, which inevitably occur during the surgical procedure, in response to surgical manipulation (resection, retraction, CSF leakage) and administration of anesthetic drugs. These changes in brain spatial configuration, summarized under the generic term of brain shift, occur according to a non-linear pattern and lead to significant mis-registration between pre-operative image data (MR, CT) and the intraoperative brain configuration. Non-rigid registration techniques are increasingly being employed to maintain an accurate alignment between pre-operative and intra-operative images. These techniques provide the ability to estimate transformations that model not only affine parameters (global translation, rotation, scale and shear), but also local deformations. Higher-order transformation models, with increased number of parameters and significant computing capabilities are usually required for this purpose. Our group was the first to demonstrate the feasibility of a non-rigid registration approach capable to compensate for the volumetric brain deformations within the time constraints imposed by neurosurgery ([Archip et al., 2007](#)). Augmented reality visualizations of functionally eloquent brain structures (based on pre-operative anatomic, functional and Diffusion Tensor MRI, non-rigidly registered with





People

- Mark Anderson
- Necu Archip
- Don Genoa
- Daniel Goldberg-Zimring
- Marianna Jakab
- Haiying Liu
- Wendy Plesniak
- (Jeff Stohll)
- Raul San-Jose
- Kinh Tieu
- Kirby Vosburgh
- Sandy Wells

