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Institute for Clinical and Translational Research

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THE HARVARD CLINICAL
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SCIENCE CENTER

Principles of medical imaging data acquisition, registration, visualization and segmentation

Randy L. Gollub, MD, PhD
MGH Departments of Psychiatry & Radiology

September 30, 2009

CTSA CLINICAL & TRANSLATIONAL
SCIENCE AWARDS

RSNA®

Radiological Society
of North America
Founded in 1915

Fundamentals of Image Processing for Extraction of Quantitative Metrics

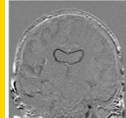
- Anatomic (volume, label)
- Functional (DCE-MRI, fMRI or PET activation)



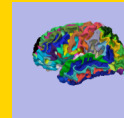
Acquire



Visualize



Register



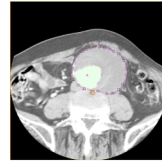
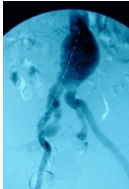
Segment
(and more...)

Available, reliable, reproducible, automatic or semi-automatic methods for each step.

Visualization



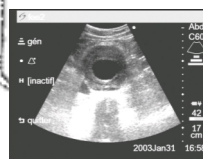
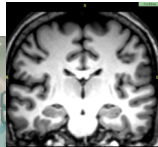
X-Ray Fluoroscopy



Computed Tomography

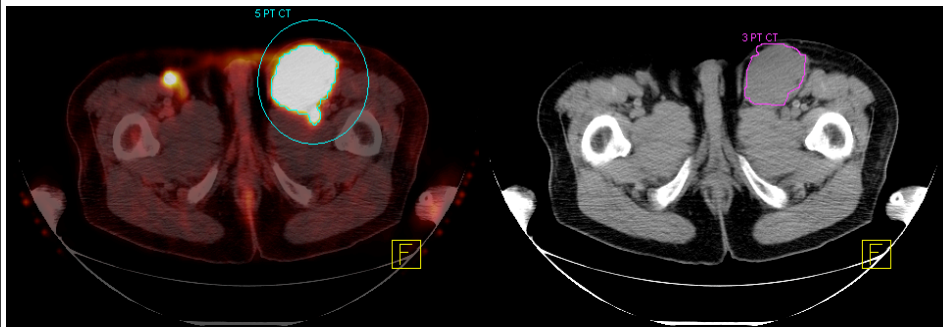


Magnetic Resonance Imaging



Ultrasound Imaging

Matching Image Acquisition Parameters to Target Biomarker

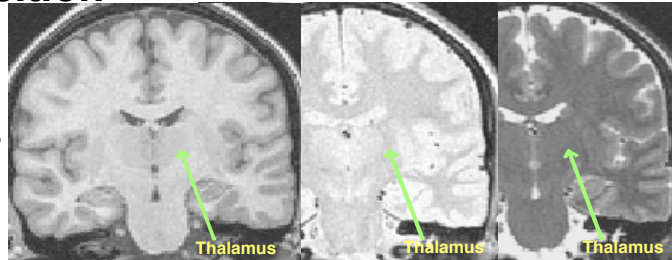


Primary outcome measures determine details of acquisition and analysis

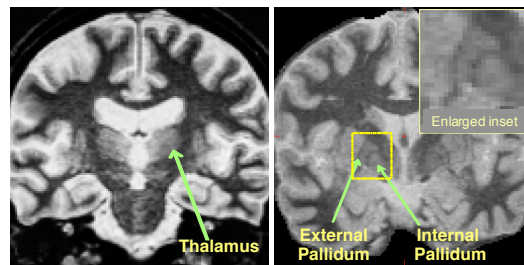
Example: Advances in Structural MRI

Image acquisition

- Traditional pulse sequences



- Novel pulse sequence improves subcortical region



Fischl et al., 2006

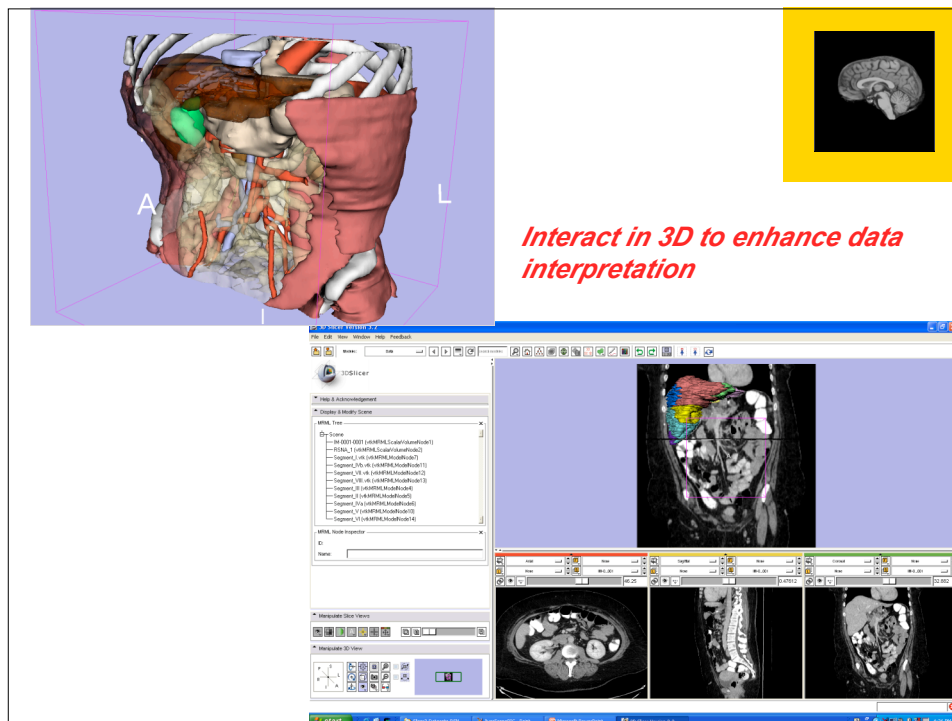
Acquisition Standardization Issues

- **Within site**
 - Across hardware/ software upgrade
- **Across sites**
 - Across vendor, platform, (field strength)
- **Longitudinal**

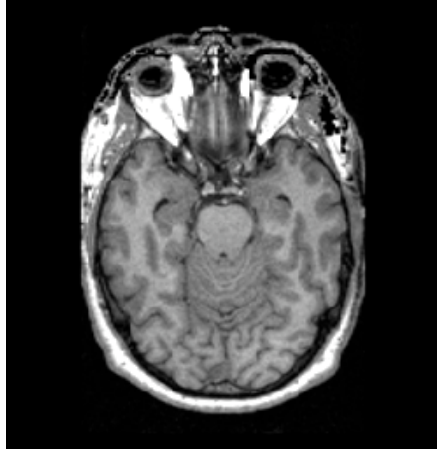
Challenges of Advances in Image Acquisition

- Subtle (and not so subtle) differences in scanner platform
- Compliance with acquisition protocol
- Need for multi-modal registration
- Increased resolution results in increased sensitivity to error contributed by image acquisition and analysis methods

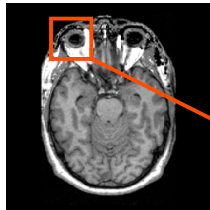
6



What is an image ?



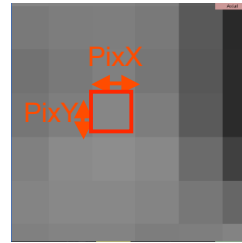
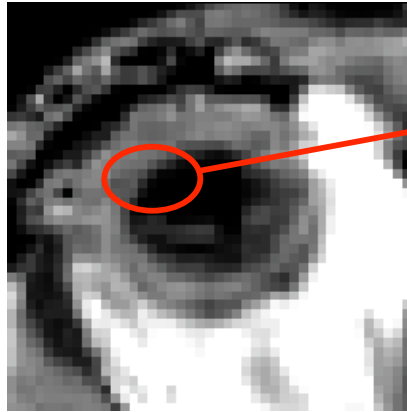
What is an image ?



2D array
of pixels

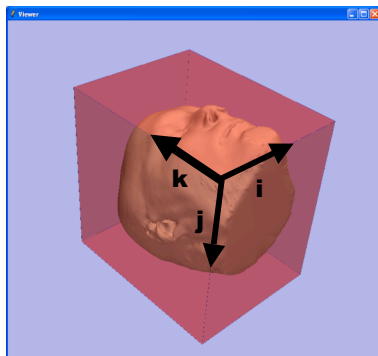


Pixel Dimensions

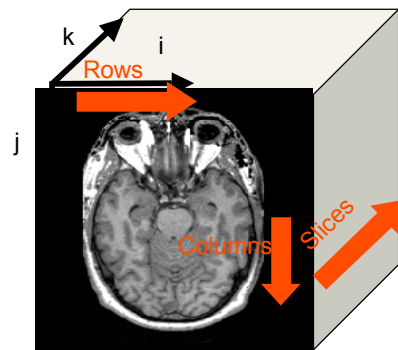


The pixel size is the dimension in millimeters of the pixels.

Data Representation

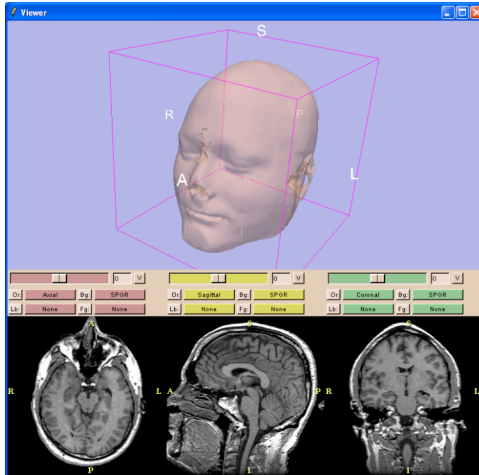


The result of the acquisition is a 3D Volume of data related to the patient.



The 3D volume is sampled on a 3D grid in the acquisition coordinate system (I,J,K).

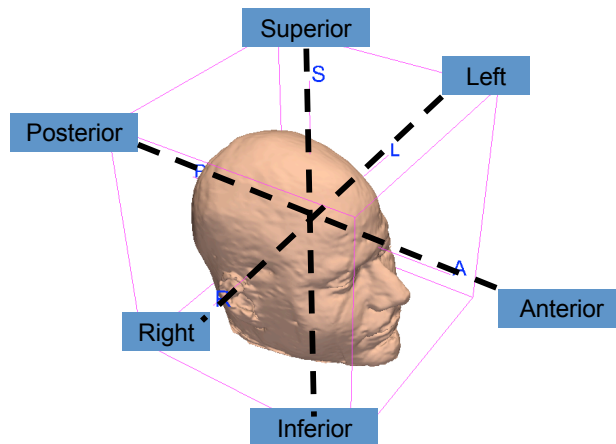
Anatomical Planes



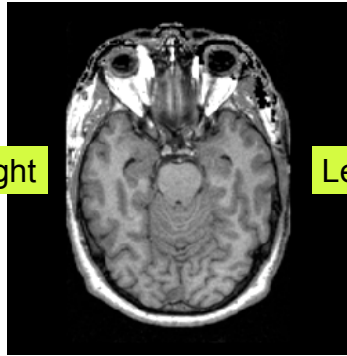
A 3D Viewer displays a model of the head.

The 2D Viewers display the three anatomical planes (axial, sagittal, coronal).

Space Directions



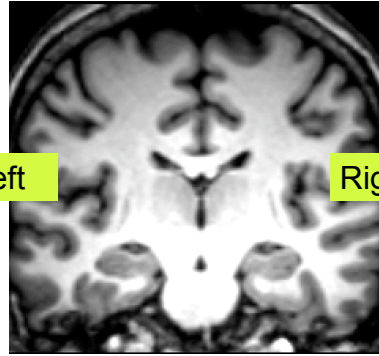
Space Orientation



Right

Left

Left

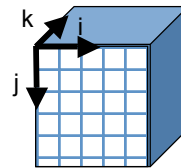
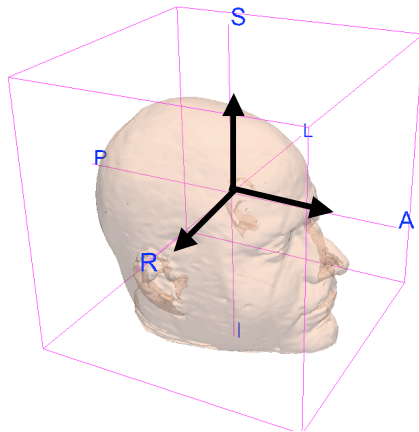


Right

Axes for Spatial Coordinates



RAS: Right-Anterior-Superior



The index i in the file increases from the Left to the **Right** side of the Patient.

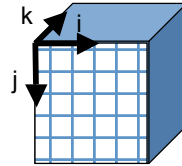
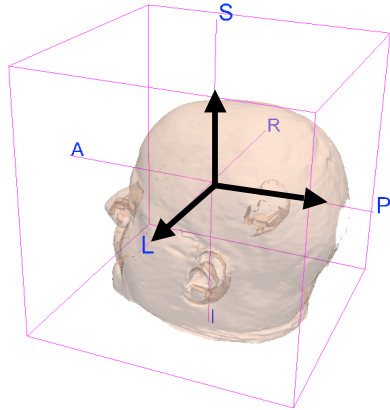
The index j in the file increases from Posterior to **Anterior**.

The index k in the file increases from **Inferior** to Superior.

Axes for Spatial Coordinates



LPS: Left-Posterior-Superior

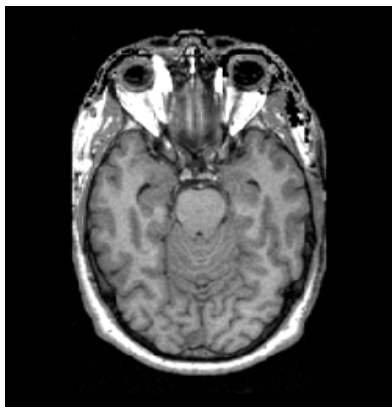


The index *i* in the file increases from the Right to the **Left** side of the Patient.

The index *j* in the file increases from Anterior to **Posterior**.

The index *k* in the file increases from Inferior to **Superior**.

DICOM 3.0 Standard



Example of DICOM header content

```
0002.0000,File Meta Elements Group Len=148
0002.0001,File Meta Info Version=256
0002.0002,Media Storage SOP Class UID=1.2.840.10008.5.1.4.1.1.4.
0002.0003,Media Storage SOP Inst UID=0.0.0.0.
0002.0010,Transfer Syntax UID=1.2.840.10008.1.2.1.
```

```
...
0008.0060,Modality=MR
0008.0070,Manufacturer=GE MEDICAL SYSTEMS
0008.0080,Institution Name=1852796513
0008.0081,City Name=1852796513
0008.0090,Referring Physician's Name=1852796513
0008.0092,?=1852796513
0008.0201,?=0500
0008.1010,Station Name=1852796513
0008.1030,Study Description=anon
0008.103E,Series Description=anon
0008.1040,Institutional Dept. Name=1852796513
0008.1050,Performing Physician's Name=1852796513
0008.1060,Name Phys(s) Read Study=1852796513
0008.1070,Operator's Name=anon
0008.1080,Admitting Diagnosis Description=1852796513
```

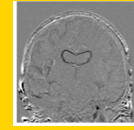
Image information

```
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0010.0020,Patient ID=1852796513
0010.0030,Patient Date of Birth=00000000
0010.0032,Patient Birth Time=000000
0010.0040,Patient Sex=O
0010.1010,Patient Age=000Y
```

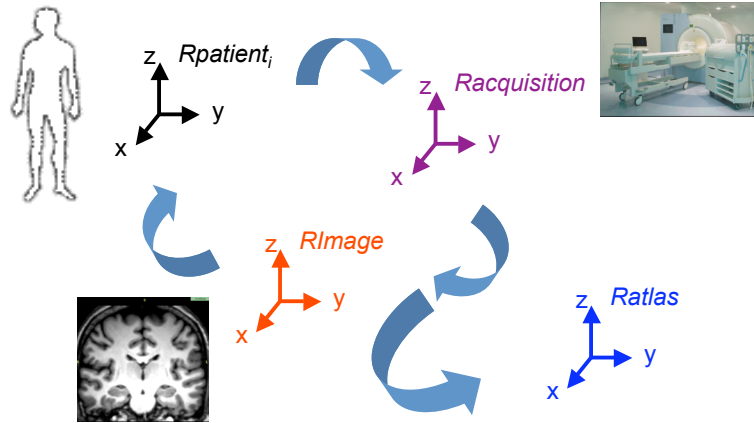
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0028.0010,Rows=256
0028.0011,Columns=256
0028.0030,Pixel Spacing=0.937500 0.937500
0028.0100,Bits Allocated=16
0028.0101,Bits Stored=16
0028.0102,High Bit=15
0028.0103,Pixel Representation=1
```

```
.....
7FE0.0010,Pixel Data=131072
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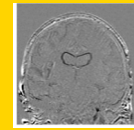
Registration



Registration is the process of transforming these three different spaces into a common reference frame



Patient \rightarrow Image Transform



Patient Space

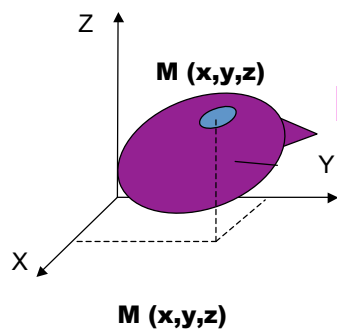
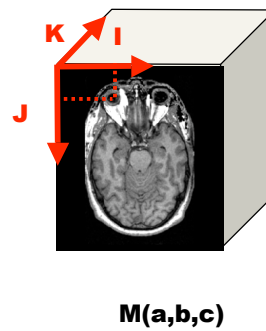


Image Space



$T_{patient \rightarrow Image}$

Uses for Image Registration

Within or Intra-subject: images acquired at near or same time

Purpose: to combine functional and anatomical information of different imaging modalities

Examples: CT and MR for surgical planning

MR and PET/SPECT images of tracer uptake for localization of functional activity

Across or Inter-subject:

Purpose: To assess individual or group variability in some anatomical or functional measure

Examples: Responders vs. non-responders to treatment

Serial or Longitudinal: a sequence of images collected over time of the same subject(s)

Purpose: To assess change within a subject or group over time due to development, aging, disease progression and/or to monitor response to treatment.

Examples: Deformation based morphometry (months), fMRI (minutes)

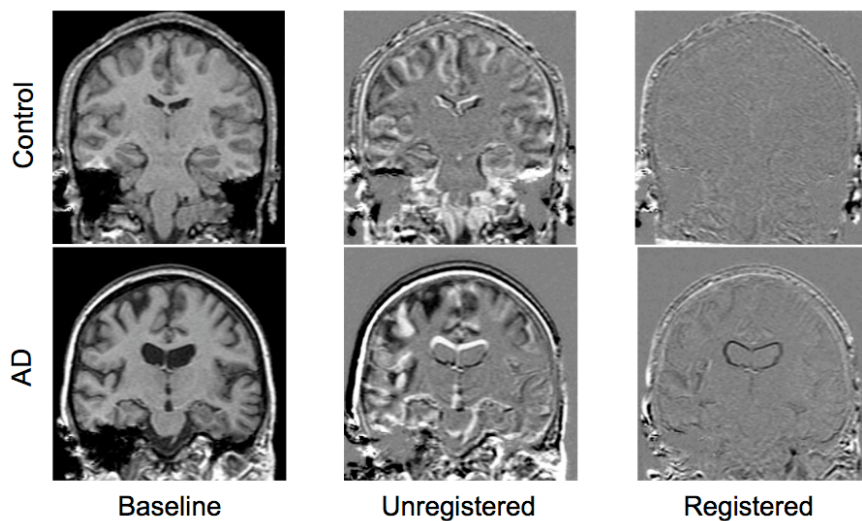
Subject to atlas:

Purpose: To use population based information as priors to inform labeling or registration

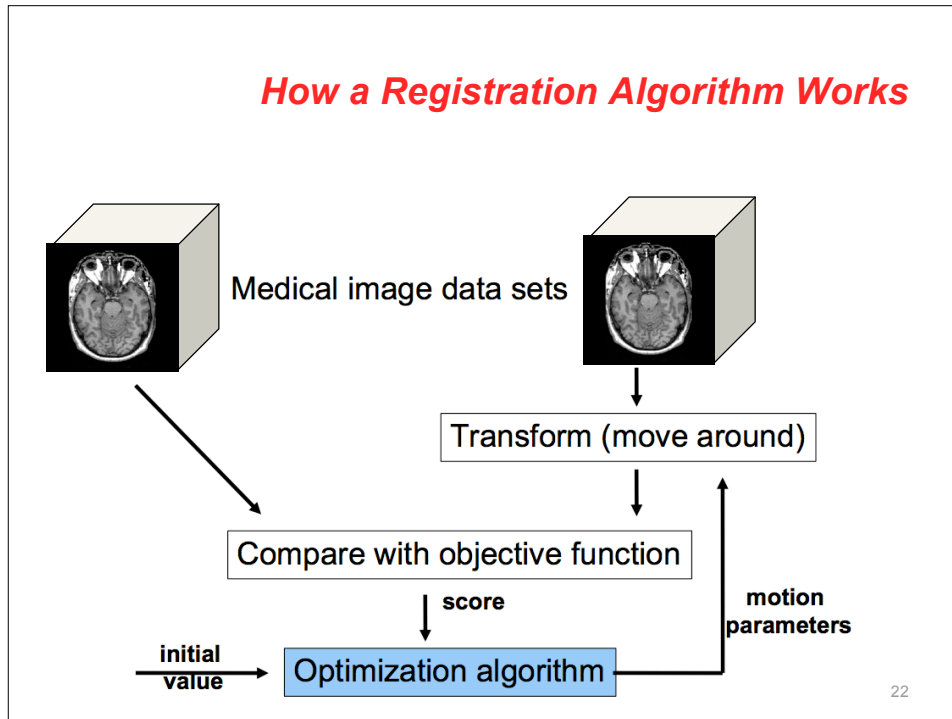
Examples: Brain segmentation and parcellation, Boundary based registration

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Why use registration? (two time points, same subject)



How a Registration Algorithm Works

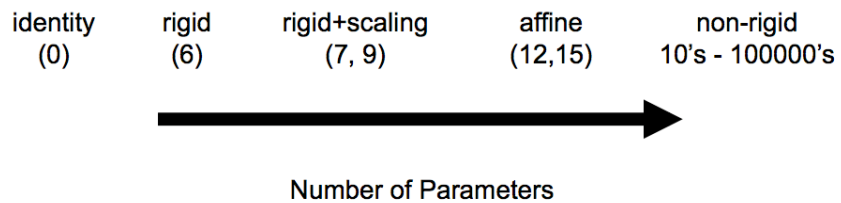


What Characterizes a Registration Algorithm?

- 1) Similarity metric (objective function): Sum of Square Differences (SSD), MSD, Normalized Correlation Ratio (n)CR, Normalized Correlation Coefficient (n)CC, Mutual Information (MI), ...
- 2) Transformation: affine, piecewise linear, nonlinear ...
- 3) Regularization: multi-resolution/scale, Gaussian blur, ...
- 4) Optimization algorithm: simplex, gradient descent,
- 5) Interpolation: nearest-neighbor (for label maps), trilinear, cubic, sinc, ...

Transformation Models

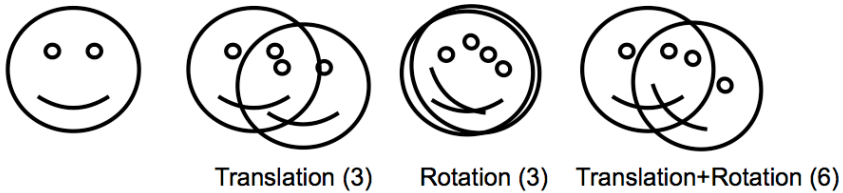
Transformations are described by the number of parameters (often referred to as Degrees of Freedom or DOF)



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Rigid-body Transformation

- Compensates for global patient repositioning
- Preserves distances, planes and angles.

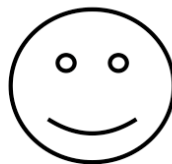


- Appropriate for:
 - brain, bone, optically tracked surgical instruments
 - often used to initialise non-rigid registration

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Affine Transformation

- Compensates for additional global size changes and shears

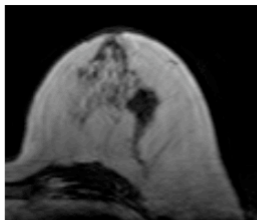


Scaling (3)

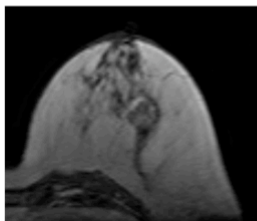


Shear (3+3)

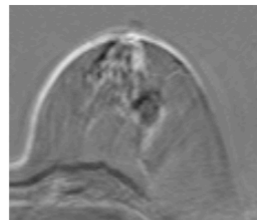
Non-rigid Transformation



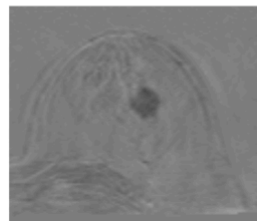
Pre-contrast



Post-contrast



Subtraction of pre- and post-contrast



Subtraction of pre- and post-contrast
after non-rigid registration

Challenges for Image Registration

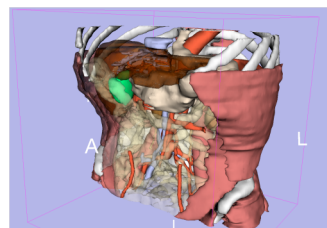
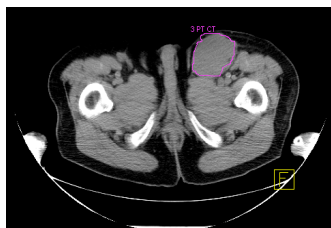
- Matching the spatial scale of the tissue of interest (e.g. cortical thickness 1-5 mm)
- Image intensity inconsistencies
 - Contrast difference (e.g. T1 vs T2 MRI)
 - Distortion differences (e.g. EPI MRI vs MRI or PET)
- Image intensity inhomogeneities (e.g. due to receiver coil characteristics)

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Segmentation Goals

Identify or label structures present in the image for:

- Quantitative measurement of volume, shape or location
- Provide boundary for visualization by surface rendering



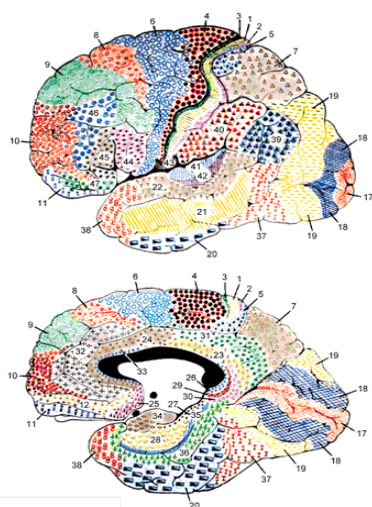
29

Segmentation Methods

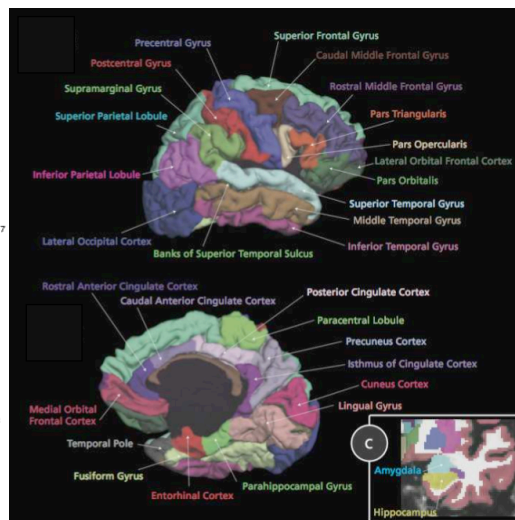
- **Interactive or manual delineation**
- **Supervised approaches with user initialization**
 - Thresholding
 - Clustering
 - Region growing
 - Edge detection
- **Atlas based alignment with a template**
- **Statistical pattern recognition**

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Structural localization of function

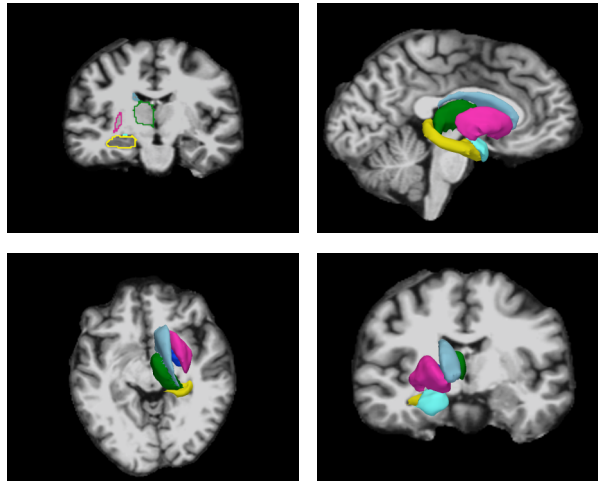


Brodmann
1909



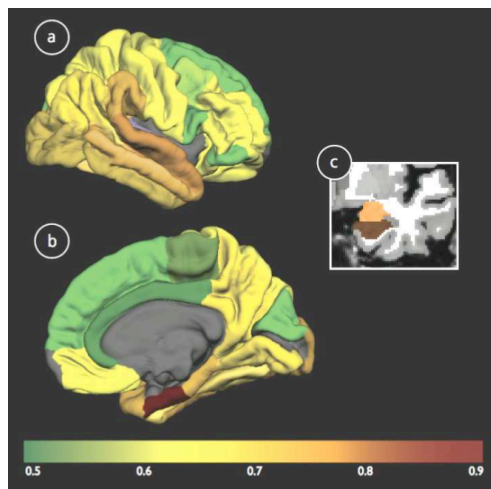
Desikan
2009

Automatically segmented structures



Freesurfer subcortical segmentation of the putamen, thalamus, hippocampus, amygdala, and caudate. Image constructed using Slicer 2.7 (www.slicer.org).

Automated Freesurfer segmentation output predicts MCI



- Entorhinal cortical thickness
- Hippocampal volume
- Supermarginal gyrus thickness

Desikan, et al in press, Brain

Technical Validation of Registration

Robustness:

Measurement precision

Consistency:

Circular (invertible) transformations

Visual assessment:

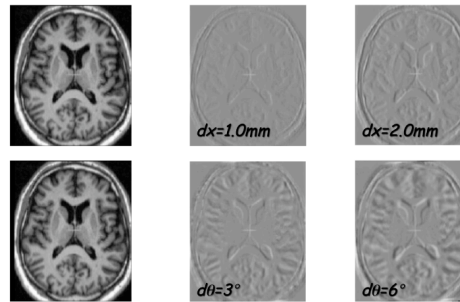
Subtraction images, overlays, landmarks

Gold Standard:

Implanted/attached markers, landmarks

Simulation of ground truth:

misregistration followed by motion recovery



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Validation of Registration, Segmentation or any Image Processing Method

Prior to entering clinical practice:

Technical validation

Speed, robustness, accuracy, reliability

Clinical validation

Utility, improved diagnosis and patient management

FDA approval, incorporation into commercial system (?)

Liability

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Acknowledgements



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Simon Warefield, PhD (CHB)



National Alliance for Medical Image Computing

NIH U54EB005149

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